

Nanostructured micronized solid dispersion of crystalline-amorphous metronidazole embedded in amorphous polymer matrix prepared by nano spray drying

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Abstract

In this study metronidazole drug was encapsulated by hydroxypropyl methylcellulose and polyvinylpyrrolidone polymers from solutions using nano spray drying technology. The influence of the process parameters and formulation variables were investigated on product morphology and structure, production yield and entrapment efficiency. The use of surface active admixtures (polyvinyl alcohol, Tween80 and Pluronic F68) increased the product yield substantially. The entrapped metronidazole was partially in crystalline and amorphous state in both amorphous polymers as confirmed by DSC and powder X-ray diffraction measurements. In the composites with hydroxypropyl methylcellulose the degree of crystallinity was between 50.2 and 81.0 %, and with polyvinylpyrrolidone between 35.0 and 50.0 % (with respect to the drug content). Melting point decrease phenomena was observed by differential scanning calorimetry between bulk metronidazole and spray dried products. Peak broadening was indicated by powder X-ray diffraction measurements, which could be the result of formation of small drug crystallites. The TEM images showed beside the larger crystals (200 – 400 nm) a fraction of smaller crystals (20 – 50 nm in diameter), which are in good correlation with the

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calculated coherent scattering domain sizes of 19 – 87 nm based on X-ray data. The drug-polymer composites produced by nano spray drying process were identified as crystalline-amorphous nanostructured micronized solid dispersions.

Keywords: nano spray dryer, solid dispersion, crystalline-amorphous nanocomposite, melting point decrease, peak broadening

1. Introduction

The spray drying process for producing powders from different fluids is well known with applications ranging from powdered milk to bulk chemicals and pharmaceuticals [1]. The use of spray drying in the pharmaceutical industry has several targets, for example manufacturing of active pharmaceutical ingredients, excipients and different solid formulations, microencapsulation, drying of heat sensitive materials and production of amorphous solid dispersions (ASD) and nanocomposites [2]. Drug nanocomposites are nano crystal based particulate systems in which the drug is usually dispersed in a polymeric matrix as a secondary phase in the form of nanocrystals [3]. Nanocomposites are often produced by one or more consecutive steps: 1) nanosuspensions preparation by high-pressure homogenization, wet media milling or nanoprecipitation, 2) drying of nanosuspension to obtain solid particles [4]. Spray drying is one of the process used for stabilization of nanosuspensions. Spray drying is a continuous process in which the drug and the excipients (stabilizers as polymers, polyelectrolites and surface active agent) are dissolved or suspended in a common solvent and the resulting solutions or nanosuspensions as well as emulsions are atomized into a drying chamber [5]. Generally, nanosuspension based drying results in nanocomposites, and solution based drying provides amorphous solid dispersion formation, although the process conditions and the composition of the suspension/solution affect the solidification process, i.e. the solid state of composite particles. Rahman et al. [6] prepared different composites with polymer

1 carriers (hydroxypropyl cellulose and Soluplus) of griseofulvin by spray drying. Spray drying
2 process was in parallel carried out with nanosuspension and solution of gresofulvin using the
3 same concentration of drug and excipients (polymers and surface active agent sodium dodecyl
4 sulphate). The experiments resulted in ASD products as a consequence of solution based drying.
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6 They found that the drying from nanosuspension produced partially amorphous products, so
7 called hybrid nanocrystal–amorphous solid dispersions (HyNASDs). The amorphous part was
8 increased by elevated polymer content and was dependent on the polymer type [6].
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11 To produce nanoparticle by spray drying, the Nano Spray Dryer B-90 is an innovative
12 equipment introduced to the market by Büchi Labortechnik AG [7, 8]. Comparing the main
13 characteristics between conventional and nano spray dryer, some features are particularly
14 relevant for expensive drug material formulations in the early development phase. The total
15 yields in a traditional spray dryer is up to 50%–70%, at least 30 mL of the solution/suspension
16 is required for a feasibility study. The forming particle size using ultrasonic nozzle is between
17 10-60 μm [5]. The nano spray dryer works with the two following unique features:
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20 a) The droplets are generated through a piezoelectric driven actuator operating at a specific
21 ultrasonic frequency. A perforated stainless steel membrane with micron-sized holes (4.0, 5.5
22 or 7.0 μm) is vibrated producing sprayed droplets with very narrow size distribution, and then
23 submicron size products.
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25 b) The submicron or micron sized particles are collected by an electrostatic collector on the
26 electrode surface, from which the fine powder product can be removed using a rubber spatula.

27 In contrast to the common cyclone technology in which the particles smaller than 2 μm are
28 typically not captured [9], this new technology enables the production of submicron- and
29 nanosized particles from 300 nm and small amount of samples (from 2 ml liquid) even with 90
30 % yield.
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1 The main process parameters of the nano spray dryer are the inlet gas temperature and flow
2 rate, the spray membrane mesh size, the feeding rate (controlled by spraying % and pump rate)
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4 [7]. As formulation variables, the main properties of materials are the solvent and excipient
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6 type, concentration and composition of the solutions, solubility of the active ingredient and
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8 excipients. The particle size, morphology, solvent residue, solid state (crystallinity and
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10 amorphous phase), entrapment efficiency and yield can be controlled by these process
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12 parameters [10]. The structure and thus the stability and the biological activity of dried products
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14 can be altered by changing the process conditions and formulation variables (solution
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16 properties) [5, 7].
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22 Metronidazole (MTZ), 2-(2-methyl-5-nitro-1H-imidazol-1-yl) as model drug and
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24 hydroxypropyl methylcellulose (HPMC) and polyvinylpyrrolidone (PVP) water soluble
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26 polymers were selected for spray drying experiments. The selected carrier polymers were
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28 significantly different in chemical structure and viscosity. MTZ is an active agent of the
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30 imidazole group drugs with wide range of bactericide effect [11]. Presently, MTZ is available
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32 in tablets, infusion and suppositories dosage forms [12]. Conventional spray drying process was
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34 used for preparing MTZ containing drugs for different administration routes [13-24].
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40 Spray drying is an energy intensive process with a very short drying time, which facilitates the
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42 generation of ASDs. However, it is also a process with several adjustable parameters, which
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44 have a determinate impact on the product quality. Dependent on the process- (drying gas
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46 properties, feed rate, nozzle type) and formulation parameters (excipients, concentration,
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48 viscosity, surface tension) and the solidification characteristics of the components, different
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50 type of amorphous and/or crystalline solid dispersion can be obtained [25, 26]. Formation of a
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52 crystalline form of the active ingredient can be attributed to its high crystallization tendency.
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54 MTZ exists in stable crystalline form [27], polymorphism has not been reported for the
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56 metronidazole base [28]. However, some authors reported partially amorphous products
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1 obtained by spray drying. Noheman et al. [14] prepared floating MTZ containing microparticles
2 using chitosan/HPMC/sodium bicarbonate in aqueous dispersion by a MSD 1.0 model mini
3 spray dryer (LMLabmaq, Brazil). The particle size (according to the SEM images) was between
4 1-10 μm , entrapment efficiency 26-43 % depending on the composition of the solutions.
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6 According to XRD pattern, the microparticles was in a semi-amorphous state, but the MTZ was
7 crystalline. Lee et al. [15] prepared Arabinoxylan microspheres by spray drying and ionotropic
8 gelation to retard the drug release of metronidazole. The drug loading was between 29.3 and
9 32.5 %, the obtained microspheres were aggregated with an individual particle size under 50
10 μm (according to SEM images). The X-ray diffraction pattern showed the MTZ peaks
11 disappeared indicating the amorphous state of the drug. Oh et al. [24] microencapsulated MTZ
12 in polyethylene glycol 3350 (PEG) using hydroxypropyl methylcellulose K15M as additive in
13 spray congealing experiment carried out in Mobile Minor™ 2000 (GEA Niro, Denmark)
14 apparatus. The author investigated the influence of K15M on the crystallinity of MTZ and
15 together with other formulation additives on drug release. They found that spray-congealing
16 with PEG reduced the crystallinity of MTZ and addition of K15M strengthened this effect. The
17 authors stated that MTZ in the microparticles (size range 33-275 μm) existed in different solid
18 state, as crystalline or amorphous particles, as well as a molecular dispersion dependent on the
19 composition of the samples. The MTZ content was rather low under 10% in the experiments.
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22 The amorphous or crystalline state of the drug and carrier and the arrangement, i.e. the structure
23 of the dispersion are very important to understand the solubility and bioavailability of the spray-
24 dried products. In the sited publications the amorphous state of MTZ in composites was
25 reported but not in detail concerning the structure of the microparticles and the effect of process
26 and formulation variables on the crystalline/amorphous state of the drug. Our aim was to study
27 the nano spray drying products concerning the possible nanostructured composition and the
28 effect of process parameters and formulation variables on the structure of MTZ–polymer solid
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1 dispersions (nanocomposites, amorphous solid dispersion). Beside the amorphous or crystalline
2 state of the active ingredient, particle size and morphology were also investigated to get
3 information about the structure of the obtained micronized solid dispersions. The production
4 yield and entrapment efficiency were determined from economic point of view.
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10 **2. Experimental**

11 **2.1. Materials**

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18 Metronidazole (T_m : 159–163 °C) [29] was a kind gift from Egis Pharmaceuticals PLC,
19 Hungary. Hydroxypropyl methylcellulose (Methocel E5, T_g : 154 °C) [30] and
20 polyvinylpyrrolidone ($M_w = 40,000$, T_g : 168 °C) [30] were purchased from Colorcon Ltd and
21 Alfa Aesar, respectively. Tween 80 was a product of Merck Schuchardt OHG. Pluronic F68
22 (T_g : 63.4°C and T_m : 54°C) [31] and polyvinyl alcohol ($M_w = 30,000-70,000$, T_g : 70°C) [32]
23 were delivered by Sigma-Aldrich Inc, Hungary.
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33 **2.2. Drying experiments**

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37 The drying experiments were carried out using a Nano Spray Dryer B-90 (Büchi Labortechnik
38 AG, Flawil, Switzerland). The basic principle of the operation of the dryer is detailed elsewhere
39 [33], the schematic setup can be seen in Fig. 1.
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44 Briefly: The preheated gas enters on the top of the chamber. The solution, nanosuspension or
45 nanoemulsion are pumped to the spray head where the ultrasonic driven atomization takes place
46 via vibrating metal membrane providing ultrafine droplets of the liquid. The droplets solidify
47 via solvent evaporation and the dried particles are collected by the electrostatic collector from
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57 The operation conditions were as follows: inlet temperature was 100, 110 or 120 °C, at a flow
58 rate of 90, 100 or 120 L/min, and mesh of the membrane was 7 μm (except experiment M where
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1 it was 5.5 μm), the recirculation pump rate was adjusted to 1. The spraying rate was not
2 independent from the solution viscosity, surface tension, the drying temperature and flow rate
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4 of the air. Generally, its ratio was chosen for 30 % but in some cases, it had to be modified to
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6 reach stable drying conditions, i. e. atomization of the solution. The drying experiments were
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8 carried out in aqueous solutions using the tall set-up constructed for water based samples
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10 ensuring enough retention time for evaporation of water. For the experiments 100 ml of
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12 solutions were prepared as followed: the solid components and the MilliQ water were weighed
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14 on analytical scale and the solutions were prepared by magnetic stirring and used without
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16 filtering. The operation conditions, the composition of the solutions to be dried are summarized
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18 in Table 1.
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24 **2.3. Characterization of powders**

25 *Morphology*

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28 Surface morphology of the samples (M, MH1 and MH2) was examined by a Philips XL30
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30 ESEM (Fei Company: Hillsboro, Oregon, USA) scanning electron microscope. The images
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32 were taken using 20 kV accelerating voltage after the samples were sputter coated with gold.
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34 Samples MH3, MH4 and MPP1 were investigated with a FEI Thermofisher Apreo S (Thermo-
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36 Fisher Scientific, Waltham, Massachusetts, USA) scanning electron microscope. In this case,
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38 the samples were not gold coated and 5 kV accelerating voltage was used.
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46 *Viscosity measurements of the solutions*

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48 Viscosity was measured on an A&D Vibro Viscosimeter (Tokyo, Japan) at 25 °C. The
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50 compositions of the solutions can be seen in Table 1 and the viscosity of the solutions in Table
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Active ingredient content and entrapment efficiency

The active ingredient content in the dried samples was determined by spectrophotometric method. For the investigations a T80 + UV-VIS spectrophotometer from PG Instruments Ltd (Leicestershire, UK) was used. To determine the amount of active ingredient content in the samples containing HPMC, standard solutions were prepared in distilled water as follows: 0.025 g of MTZ was dissolved in 100 mL distilled water. 5 mL of this solution was diluted to 25 mL and further dilutions were made to concentrations of 2.5; 5; 10; 20; 30 and 40 µg/mL. The absorbance at 319 nm was measured and used for the calibration. In case of PVP containing samples, this calibration curve was not applicable because the MTZ content cannot be determined with sufficient accuracy in the presence of this polymer. To overcome this, another calibration was made in hydrochloric acid medium [34]. The solutions for the calibration were prepared in the same concentration as previously using 0.1 mol/L concentration HCl solution. The absorbance maximum at 276 nm was used for the calibration curve. For spray dried sample analysis, 10 mg product was dissolved and diluted to a concentration of 40 µg/mL. To calculate the concentration of MTZ in the dried samples, the following equations (1, 2) were used:

for samples containing HPMC:
$$C_{MTZ} = \frac{(A_{319} + 0.0019) / 0.0518}{40} \cdot 100 \quad (1)$$

for samples containing PVP:
$$C_{MTZ} = \frac{(A_{276} + 0.0008) / 0.0381}{40} \cdot 100 \quad (2)$$

where C_{MTZ} : MTZ content (w/w %) in the dried samples, A_{319} : absorbance at $\lambda = 319$ nm, A_{276} : absorbance at $\lambda = 276$ nm.

The entrapment efficiency (EE%) was calculated by equation 3 [35]:

$$EE\% = \frac{C_{MTZ}}{C_{MTZ,t}} \cdot 100 \quad (3)$$

where $C_{MTZ,t}$: MTZ amount in percentage relative to the whole solid content in the solution to be dried, i.e. the theoretical MTZ content.

Particle size and distribution

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3 The particle size and distribution were determined by laser diffraction method. The calculation
4 requires knowledge of the optical properties, such as refractive index (RI) and the imaginary
5 component (Ab) of the refractive index of the solid sample being measured. The dried products
6 are different in composition thus for the calculation RI = 1.5 and Ab = 0.1 were used as assumed
7 data because they provided eligible fit between the calculated and measured data (residual
8 shows the measured scattering data and the data predicted by the scattering model was under 1
9 % according to the Malvern Instruments Operators Guide [36]). The particle size was reported
10 as a volume equivalent sphere diameter marked as d(4,3) and the distribution with d10, d50 and
11 d90 data. The measurements were carried out in wet dispersion in 100 mL of cyclohexane
12 containing 0.1 % soy lecithin by a Malvern Mastersizer 2000 (Malvern Instruments, Malvern,
13 UK) using the SM dispersion unit with a stirring rate of 2000 rpm. 10 mg of sample was
14 weighed in 1 mL of cyclohexane solutions containing 0.1 % soy lecithin and sonicated for 40 s
15 at 30 % of power with 6 mm probe by Sonics VCX 130 instrument, then the obtained suspension
16 was poured into the dispersion unit for measurement.
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Thermal measurements

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41 Thermal measurements were performed on a Setaram LabsysEvo thermal analyser (Setaram
42 Instrumentation, Caluire-et-Cuire, France), in flowing (90 mL/min) high purity helium
43 (99.9999%), with a heating rate of 20 °C/min. On average, 5-6 mg of sample was weighed into
44 100 µL aluminium crucible and was analysed in the 25-300 °C temperature interval. The results
45 were evaluated by using Calisto Processing (version 2.0, AKTS, Switzerland) software, and
46 every measurement was baseline corrected before processing.
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X-ray diffraction measurements

X-ray diffraction images were recorded using a Philips PW 3710 diffractometer (Philips Analytical, Almelo, Netherlands) with CuK α radiation with a tube current of 40 mA and a voltage of 50 kV at a scanning rate of 0.02 ° 2 θ / s. Control of the device and data collection was done with Philips X'Pert Data Collector software.

Transmission electron microscopy (TEM)

Samples for TEM were prepared by depositing a drop of hexane suspension of sedimented particles on copper TEM grids covered by lacey carbon amorphous support film. TEM analyses were performed using a Talos F200X G2 instrument (Thermo Fisher, Waltham, MA, US), operated at 200 kV accelerating voltage, equipped with a field-emission gun and a four-detector Super-X energy-dispersive X-ray spectrometer, and capable of working in both conventional TEM and scanning transmission (STEM) modes. Low-magnification bright-field (BF) images were obtained in TEM mode.

3. Results and discussion

3.1. Entrapment efficiency, yield and particle morphology

The drying process variable parameters were the inlet temperature and flow rate of the drying air, the concentration of the active ingredient, polymer and admixtures in the solutions to be dried. The process parameters are given in Table 1 and the entrapment efficiency, yield, the active ingredient content, the volume equivalent sphere diameter (particle size) of products and the viscosity of the solutions are shown in Table 2.

The solubility of metronidazole in water is 10.6 mg/mL at 25 °C [27]. In experiment M the metronidazole was dried without carrier and additives, and its concentration was 1.0 % (w/w) close to its solubility limit. The yield was very low, and the product couldn't be removed from

1 the collecting electrode, since it was very sticky. The SEM image showed (Fig. 2A) that dried
2 active ingredient is electron beam sensitive. Excipients are often used to facilitate the
3 manufacture process of the drug or modify its biological activity. In the drying experiments
4 HPMC and PVP as different polymer carriers were used for encapsulation of the MTZ.
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10 The concentration of HPMC in MH1 – MH10 experiments was adjusted to 1.0, 1.5 and 2.0 %
11 (w/w). The particles morphology was investigated using different operational parameters in the
12 experiments MH1 – MH3 (detailed data of experiment conditions are given in Table 1). The
13 particle shape and morphology are important for further processing to get a drug formula, and
14 additionally for the drug pharmacokinetics [37]. Particles with active ingredient crystals on the
15 capsule surface can suffer from a burst release, which under some circumstances can be
16 preferred or in contrary, even unwanted. In the experiment MH1 the concentration of the MTZ
17 and HPMC was similar, i.e. 1.0 % (w/w). In Fig. 2B well developed MTZ crystal size around
18 10 μm and spherical polymer particles can be seen. During the drying process, the water
19 evaporation enhanced the concentration of the solid materials in the solution. Solidification and
20 diffusion took place simultaneously, and the product morphology depended on the ratio of these
21 processes, i.e. on the solubility of materials and the viscosity of solution [33, 38]. In our case,
22 the used concentration of the MTZ was its solubility limit in water, which means that
23 supersaturation was reached suddenly during the evaporation causing crystallization of the
24 MTZ before the polymer solidified, thus the MTZ was not really encapsulated in the polymer
25 matrix. The polymer acted more as drying aid to mask the unfavourable drying characteristics
26 of MTZ. The evaporation rate is dependent also on the drying temperature. In the experiment
27 MH2 and MH3 different drying temperature was used, 120 °C and 100 °C, respectively. MTZ
28 concentration was 0.5 % (w/w), i. e. under its solubility limit and HPMC:MTZ ratio was also
29 higher than in experiment MH1. In Fig. 2C (MH2) small MTZ crystals are also observable on
30 the microcapsules surface, while in Fig. 2D (MH3) only polymer microcapsules can be seen,
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1 suggesting that the MTZ was encapsulated successfully. In case of 120 °C drying air
2 temperature, the evaporation rate is higher than using 100 °C, which resulted also in a faster
3 crystallization of the active ingredient from the solution droplets, and did not give enough time
4 for the diffusion of MTZ inside the polymer.
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10 The yield and entrapment efficiency are important for economical point of view of the process.
11 In the experiments MH4 – MH8 the drying temperature and flow rate were used in different
12 combinations: $T_{in} = 100$ and 120 °C, $V_{air} = 120, 100$ and 90 L/min. The concentration of the
13 solutions was fixed (see details in Table 1). Using 120 °C inlet temperature, the entrapment
14 efficiency and yield increased by decreasing the air flow rate (samples MH4 – MH6, Table 2.).
15 Particle size also increased from 6.36 to 10.38 μm . Experiments with 100 °C drying air
16 temperature did not show substantial difference in the two efficiencies using 90 or 120 L/min
17 flow rate (samples MH7 and MH8). In experiment H the HPMC polymer was also dried at a
18 concentration of 1 % (w/w). The highest yield and the lowest particle size was very close to the
19 values obtained for the dried sample H, i.e. the pure polymer.
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35 The polymer concentration range in the solutions is limited because of the maximum viscosity
36 of the solutions, which can be atomized by the piezoelectric generated spraying. In experiment
37 MH9 the operational limit was reached with 2.0 % HPMC concentration, i. e. 4.01 mPa*s
38 viscosity at 25 °C, the temperature also had to be adjusted to 120 °C, which resulted in higher
39 spray head temperature in accordance with decreased viscosity during spraying. In experiment
40 MH10 the MTZ concentration was increased to 0.75 % (w/w), the entrapment efficiency and
41 yield were even higher than using 0.5 % (w/w) MTZ in experiment MH3. The operational
42 parameters did not show real effect on particle size except for MH9 in which particle size above
43 20 μm was generated due to the high viscosity of the solution. The experiments with HPMC
44 indicated that an inlet temperature of 100 °C, flowing rate of drying air of 90 L/min ensured the
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1 highest entrapment efficiency and yield (see Table 2), that's why the experiments with PVP
2 were carried out at fixed inlet temperature (100 °C) and drying air flow rate (90 L/min).
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5 PVP has a wider polymer concentration range taking into account its applicable viscosity during
6 spraying. In the experiments MPP1 – MPP4, the concentration of PVP was 5.0, 2.5 and 1.5 %
7 (w/w) and that of MTZ was 0.75 and 0.5 % (w/w). It is also important to take into consideration
8 not only the total concentration of solution but also the PVP:MTZ ratio in the solutions to be
9 dried. The entrapment efficiency was above 90 % in all cases. Surprisingly, in the MPP1
10 product this value was higher than 100 %, which means the MTZ enriched in the powder. The
11 reason of this anomaly is the used high polymer ratio, from which higher amount of polymer
12 left with the drying air without being isolated by the electrostatic collector. The yield in
13 experiment MPP3 was only 16.9 %, and the particle size was particularly large (44.7 µm, see
14 in Table 2). The PVP:MTZ ratio was 2:1 which was not sufficient for masking the MTZ's
15 unfavourable drying characteristics as experienced in the experiment M. In the experiment
16 MPP4, by increasing the PVP:MTZ ratio to 3:1, the yield was similar to MPP2. Taking into
17 account also the particle size distribution (Fig. 3A), some differences could be observed
18 compared to the experiments carried out with PVP polymer. The samples with a lower
19 PVP:MTZ ratio gave a bimodal distribution showing the influence of MTZ (samples MPP3 and
20 MPP4). The higher polymer concentration resulted in higher yield.
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24 Additives such as surface active agents are capable of changing the solution characteristics
25 significantly during drying, moreover, they can influence also the dissolution profile of the
26 drug. The same composition were used in the experiments MPP2, MPP2_T, MMP2_{PA} and
27 MPP2_{PL} with different admixtures of 0.1% (w/w), namely Tween 80, PVA and Pluronic F68,
28 respectively. Using surface active agents, the entrapment efficiency was significantly higher
29 with PVA and Pluronic F68 compared to the result achieved with Tween 80. The particle size
30 was enhanced, and the size distributions were very similar in all three experiments (Fig. 3B).
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1 The yield increased in the experiments MPP2_{PA} and MPP2_{PL} by 15% and 13 %, respectively,
2 compared to the sample MPP2. The appropriate selection of a surface active agent can facilitate
3 the product collection from the collective electrode surface, resulting in higher yield. The
4 maximum achievable yield in the experiments with PVP was 78.8 % (experiment PP) where
5 the pure polymer was dried which also indicates the unfavourable characteristic of the MTZ
6 during drying.
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13 **3.2. Thermal measurements**

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18 The DSC curves show that the samples dried with polymers (Fig. 4B and C) have different
19 melting point behaviour compared to the pure MTZ or dried M sample (see Fig. 4A). In the
20 heat flow curve of MTZ and M, two peaks can be seen: the first sharp peak between 159.7 and
21 174.7 ° C corresponds to the melting of the MTZ, while the second peak (295.7 ° C) corresponds
22 to the molten material decomposition (280 ° C according to [39]). In the majority of samples,
23 the melting endotherm indicates the crystalline state of MTZ incorporated in the amorphous
24 polymer carriers (H and PP on Fig. 4A). The active ingredient content, onset and offset
25 temperatures, peak temperatures, and melting enthalpies are summarized in Table 3. MTZ and
26 M melts between 159.7 – 174.7 and 157.5 – 166.3 ° C, respectively (according to the US
27 Pharmacopeia the melting point of MTZ is between 159 – 163 ° C, [40]), whereas this melting
28 interval is located at much lower temperatures for the dried samples. The dried samples are
29 composite materials of an active ingredient and polymer(s), hence they are solid dispersions.
30 The solid dispersions can be classified into three broader groups as eutectic mixtures, solid
31 solutions and microfine crystalline dispersions [41]. To interpret the phenomena of melting
32 point decrease and to investigate the solid states of dried products, thermal data (melting
33 intervals and enthalpies) of HPMC polymer containing samples were evaluated, and compared
34 with the result obtained from powder X-ray diffraction (see section 3.3) and transmission
35 electron microscopic measurements (see section 3.4.).
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1 The selected samples in experiments carried out with HPMC had two endotherm peaks between
2 99.1 and 160.0 °C (Fig. 4 B). D. J. Blundell examined poly(ether ether ketone) by DSC and
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4 assumed two hypotheses for double melting peaks: (i) they are due to two separate crystal
5 morphologies; (ii) they are attributable to recrystallization effects [42]. P. Corradini et al.
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7 discussed the splitting of the melting peak for isotactic polypropylene. They assumed if the X-
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9 ray data indicated only one crystal form, the two different melting peaks could be attributed to
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11 different disordered crystals, different crystal sizes, or different crystal types [43]. In our case,
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13 when the total melting enthalpy values (obtained by adding the enthalpy of the two successive
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15 endotherms) were plotted against the active ingredient content (Fig. 5), a straight line could be
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17 obtained with a 15 % error bar, demonstrating that the total enthalpy was correlated to the
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19 amount of MTZ content in the samples. In case of recrystallization process, this correlation
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21 would not have existed. Comparing the enthalpy of the first and second melting peaks in our
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23 experiments with HPMC, their ratio in the total value changed in each experiment (Table 4, the
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25 table does not contain MH2, MH3, MH10 samples due to the increased spray rate, the outlet
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27 temperature decreased so could not be compared to other samples). It has been discussed in
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29 several papers that melting temperature of nanoparticles is dependent on the particle size [44,
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31 45]. Assuming that the melting point decreased because of the reduction of crystal size, the first
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33 endotherm corresponded to the melting of smaller crystals, while the second larger endotherm
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35 was the result of melting of the larger crystal fraction [46]. Thus, with respect to the ratio of the
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37 first peak to the second one, a higher ratio represented higher number of smaller crystals. Its
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39 reason can be explained with the different drying conditions. As mentioned above, drying is
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41 determined by two processes, firstly, by the reduction in solubility due to solvent evaporation
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43 leads to solidification of the product and secondly by the rate of diffusion. The ratio of the
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45 solidification to the diffusion rate depends on the followings:
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- 59 - concentration of material in the solutions (concerning its solubility),
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- viscosity of solutions,
- the drying temperature determined from inlet temperature and air flow rate.

The crystal formation is demonstrated in Fig. 6. The lowest ratio of 0.02 was obtained for MH1 sample. Adjusting the concentration of MTZ to 1 % (w/w) that is its solubility limit, the crystallization took place very fast, and most of the crystals in bigger size grew outside the polymer drops (Fig 2B). The highest ratio was reached at sample MH9 with a value of 0.72 using the highest polymer concentration (2 %), which favours the formation of smaller crystals. Increasing the polymer concentration, therefore the viscosity of the solution, resulted in lower diffusion coefficient, thus causing the formation of smaller crystals. In other cases the ratio of the solidification and diffusion was mainly determined by the drying temperature. The higher the temperature, the faster solidifying the particles and diffusion could not occur, producing smaller crystals. Furthermore, the drying air flow rate had also influence on the solidification and diffusion rates. Shorter evaporation time was the consequence of its higher rate in higher outlet temperature resulting in also smaller crystals. The variation in the ratio of two peaks correlated with the change of the operational parameters, thus, this also proved that both peaks corresponded to the melting of the MTZ.

In the case of samples dried with PVP excipient, two different melting points were not obviously separated on the DSC curves. The reason can be the different interaction between MTZ and HPMC or PVP, or the different solidification process of the polymers (Fig. 7). The shape of the particles with HPMC polymers was collapsed hollow spheres, while the composites was spherical with PVP.

The degree of crystallinity was examined in comparison with the active ingredient content (data in Table 5). The MH4 sample gave the lowest degree of crystallinity relative to the active ingredient content (50.2 %), while the MH1 sample the highest (87.1 %). In the case of MH1 sample, this ratio is high because of the relatively large amount of active ingredient compared

1 to the polymer, therefore only a small ratio of MTZ was generated in amorphous form. In the
2 case of MH4 sample, this ratio is the lowest because the drug crystallized rapidly during the
3 drying due to the high temperature and air flow rate forming more amorphous MTZ. On the
4 other hand, most of the crystals were removed by the drying air from the surface of the particles,
5 reducing the amount of crystalline drug compared to the amorphous drug.
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11 For samples containing PVP, the degree of crystallinity varied between 35.0 and 50.0 % (not
12 calculated for MPP1 and MPP2 samples due to inadequate fitting). The reason for it was the
13 PVP polymer was used in larger amounts due to its lower viscosity, the ratio of polymer was
14 higher than in the HPMC-containing samples.
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22 If only the degree of crystallinity was taken into account, its value moved from 9.1 % (MH4)
23 to 43.6 % (MH1), and from 7.6 % (MPP2_{PL}) to 13.2 % (MPP4) for samples containing HPMC
24 or PVP (not calculated for MPP1 and MPP2 samples), respectively.
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30 ***3.3 X-ray diffraction measurements***

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32 The DSC curves showed that MTZ had a well-defined melting point in the most of the samples,
33 that is, a part of the active ingredient was encapsulated surely in crystalline state in the
34 amorphous polymer providing a form of solid dispersion. The powder X-ray diffraction results
35 also confirmed the crystalline state of the MTZ (Fig. 8A and B) except sample MPP1 in which
36 the MTZ content was the lowest. Peak broadening can also be seen compared to the pure MTZ
37 (Fig. 9 in case of MPP4 sample). The results are listed in Table 6 for selected MTZ products.
38
39 The possible reason for peak broadening is the decrease in crystal size relative to the bulk MTZ
40 [47, 48]. As discussed in section 3.2, based on the results of DSC investigations of the dried
41 samples, they showed reduced melting point compared to the bulk MTZ. The decrease in
42 crystallite size accompanies with the drop of melting point as discussed also by Roumanille et
43 al. [49] in case of bismuth oxalate nanoparticles. According to the Scherrer equation, the
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calculated coherent scattering domain sizes were in the range of 19 – 87 nm (Table 6), which was also confirmed by the TEM measurement results (see section 3.4). According to the degree of crystallinity relative to the amount of the drug and the results of X-ray measurement, it can be stated that the drug was partially in crystalline and amorphous state in the amorphous polymer.

3.4 TEM investigations

Scanning transmission electron microscopic images of sample MH2 were imaged in bright field mode (Fig. 10). Due to the fact that the focused beam of high-energy electrons damaged most of the investigated samples, reliable images were taken only from sample MH2. The small MTZ crystals appeared as dark spots, because they are scattering much more electrons than the amorphous polymer that does not have long range order. On lower magnification in Fig. 10A and B the crystallite sizes were between 200 – 400 nm in diameter. In higher magnification smaller MTZ crystals became visible (Fig. 10 C and D), and their sizes were between 20 – 50 nm in good agreement with the calculated domain sizes obtained from the X-ray measurements (the data is given in Table 6). Based on these results, we can conclude that the spray dried MTZ-polymer composite products were nanostructured solid dispersions in which the drug was distributed in crystalline and amorphous form in the polymer matrix [50]. Size stabilized nanostructured drug microparticles have been often produced by two or more consecutive steps, e.g. by direct spray drying of the nanoprecipitated budesonide-mannitol composites, microparticles were prepared as reported by Hu et al [51]. In our experiments the nanostructured product was formulated by a one-step spray drying process.

4. Conclusions

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4 In the present work, MTZ active ingredient was encapsulated in HPMC and PVP polymers
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6 from solutions by nano spray drying technology. The concentration of active ingredient and
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8 polymer as well as their relative ratio had a significant influence on the process feasibility, since
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10 the concentration of polymer defines the solution viscosity and the solubility relations. During
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12 drying, the solidification and the diffusion occurred simultaneously, while the product
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14 morphology depended on the ratio of these processes, e. g. the MTZ could not be fully entrapped
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16 into the polymer matrix, when its concentration was adjusted to the solubility limit. In the
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18 micron-sized dried products, the entrapped MTZ was in partially crystalline and amorphous
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20 form in both polymers as confirmed by DSC and powder X-ray diffraction measurements. The
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22 degree of crystallinity was between 50.2 and 81.0 % and between 35.0 and 50.0 % in HPMC
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24 and in PVP composites, respectively (with respect to the drug content), dependent on the
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26 solution composition and process conditions. The crystalline state of the samples with HPMC
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28 was investigated to get information about the structure of the composites. The MH samples had
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30 two endothermic peaks between 99.1 and 160.0 °C, that can be attributed to the MTZ melting
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32 process. The ratio of the first and second melting enthalpy peak changed with the drying
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34 conditions. The higher evaporation rate gave higher ratio of first and second peak, which
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36 probably can be assigned to a decrease in the crystal size resulting in the reduction of melting
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38 point. This assumption was supported by the peak broadening which was observed in the X-ray
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40 measurement. The TEM images showed larger crystals (200 – 400 nm) and a fraction of much
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42 smaller crystals (20 – 50 nm in diameter), which are in good correlation with the calculated
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44 coherent scattering domain sizes on the basis of X-ray data. The DSC, powder X-ray and TEM
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46 analysis supported the assumption that the MTZ-polymer composites were nanostructured solid
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48 dispersion in which the nanometer size crystals and the amorphous fraction of the active
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50 ingredient distributed in the amorphous polymer matrix. To keep the active ingredients in stable
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1 nanoformulation is a challenge, which might be achieved by embedding the nanoparticles into
2 polymer microparticles. Using spray drying process, nanosuspension, nanoemulsion or
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4 solutions can be transformed to solid microparticles that incorporated the active ingredient in
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6 different state (crystalline, amorphous or crystalline-amorphous) mainly in polymer matrices.
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8 To investigate the product structure is rather difficult, because the carrier and the drug often
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10 have similar characteristics concerning the different identification methods. In our case, the
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12 crystalline part of the drug formed nanstructured solid dispersions.
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17 **5. Acknowledgements**

18
19 Authors would like to acknowledge the European Structural and Investments Funds and the
20
21 Hungarian Government for providing funding in frame of GINOP-2.2.1-15-2016-00023 project
22
23 for this work. This work was also supported by the TKP2020-IKA-07 project financed under
24
25 the 2020-4.1.1-TKP2020 Thematic Excellence Programme by the National Research,
26
27 Development and Innovation Fund of Hungary. The authors are especially grateful to the EGIS
28
29 Pharmaceuticals PLC for their partnership. TEM/SEM studies were performed at the electron
30
31 microscopy laboratory of the University of Pannonia, founded with the aid of grant no. GINOP-
32
33 2.3.3-15-2016-0009 from the European Structural and Investments Funds and the Hungarian
34
35 Government. The authors express their gratitude for Éva Kristóf Makó (University of Pannonia)
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37 for the powder X-ray diffraction measurements.
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6. References

- 1
2
3
4 [1] A. S. Mujumdar, L.-X. Huang, X. Dong Chen, An overview of the recent advances in
5 spray-drying, *Dairy Sci. Technol.* 90 (2010) 211–224.
6
7
8
9 [2] R. Vehring, *Pharmaceutical Particle Engineering via Spray Drying*, *Pharmaceutical*
10 *Research* 25(5) (2007) 999–1022.
11
12
13
14 [3] A. Bhakay, M. Rahman, R. N. Dave, E. Bilgili, Bioavailability Enhancement of Poorly
15 Water-Soluble Drugs via Nanocomposites: Formulation–Processing Aspects and Challenges,
16 *Pharmaceutics* 10 (2018) 86.
17
18
19
20
21
22 [4] J. P. Möschwitzer, Drug nanocrystals in the commercial pharmaceutical development
23 process, *International Journal of Pharmaceutics* 453 (2013) 142– 156.
24
25
26
27
28 [5] S. M. Jafari, C. Arpagaus, M. A. Cerqueira, K. Samborska, Nano spray drying of food
29 ingredients; materials, processing and applications, *Trends in Food Science & Technology* 109
30 (2021) 632–646.
31
32
33
34
35
36 [6] M. Rahman, F. Arevalo, A. Coelho, E. Bilgili, Hybrid nanocrystal–amorphous solid
37 dispersions (HyNASDs) as alternative to ASDs for enhanced release of BCS Class II drugs,
38 *European Journal of Pharmaceutics and Biopharmaceutics* 145 (2019) 12–26.
39
40
41
42
43 [7] X. Li, N. Anton, C. Arpagaus, F. Bellesteix, T. F Vandamme, J., Nanoparticles by spray
44 drying using innovative new technology: The Büchi Nano Spray Dryer B-90, *Journal of*
45 *Controlled Release* 147(2) (2010) 304–310.
46
47
48
49
50
51 [8] N. Schafroth, C. Arpagaus, U. Y. Jadhav, S. Makne, D., Douroumis, Nano and
52 microparticle engineering of water insoluble drugs using a novel spray-drying process, *Colloids*
53 *and Surfaces B: Biointerfaces* 90 (2012) 8–15
54
55
56
57
58
59 [9] K. Mosen, K. Backstrom, K. Thalberg, T. Schaefer, H. G. Kristensen, A. Axelsson,
60
61
62
63
64
65

1 Particle formation and capture during spray drying of inhalable particles, *Pharmaceutical*
2 *Development and Technology* 9(4) (2004) 409–417.

3
4
5 [10] Y.-F. Maa, H. R. Costantino, P.-A. Nguyen, C. C. Hsu, The Effect of Operating and
6
7 Formulation Variables on the Morphology of Spray-Dried Protein Particles, *Pharmaceutical*
8
9 *Development and Technology* 2(3) (1997) 213-223.

10
11
12 [11] A. J. K. Atia, Synthesis and Antibacterial Activities of New Metronidazole and
13
14 Imidazole Derivatives, *Molecules* 14 (2009) 2431-2446.

15
16
17
18 [12] S. Naveed, N. Waheed, S. Nazeer, Degradation Study of Metronidazole in Active and
19
20 Different Formulation by UV Spectroscopy, *Journal of Bioequivalence & Bioavailability*, 6(4)
21
22 (2014) 124-127.

23
24
25
26 [13] M. Szekalska, K. Winnicka, Evaluation of Hard Gelatin Capsules with Alginate
27
28 Microspheres Containing Model Drugs with Different Water Solubility, *Acta Poloniae*
29
30 *Pharmaceutica - Drug Research*, 74(4) (2017) 1221-1230.

31
32
33
34 [14] L. Nohemann, M. P. de Almeida, P. C. Ferrari, Floating ability and drug release
35
36 evaluation of gastroretentive microparticles system containing metronidazole obtained by spray
37
38 drying, *Braz. J. Pharm. Sci.* 53(1) (2017) e15218.

39
40
41
42 [15] C. J. Lee, C. S. Nah, C. S. Teng, W. W. Jun, M. Saravanan, Spray dried calcium gelled
43
44 arabinoside microspheres: A novel carrier for extended drug delivery, *Chemical Papers* 69(10)
45
46 (2015) 1325–1330.

47
48
49
50 [16] Z. Vanic, O. Planinšek, N. Škalko-Basnet, I. Tho, Tablets of pre-liposomes govern in
51
52 situ formation of liposomes: Concept and potential of the novel drug delivery system, *European*
53
54 *Journal of Pharmaceutics and Biopharmaceutics*, 88(2) (2014) 443–454.

- 1
2
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65
- [17] V. Jokanovic', B. C'olovic', M. Dutour Sikiric', V. Trajkovic', Tablets of pre-liposomes govern in situ formation of liposomes: Concept and potential of the novel drug delivery system, *Ultrasonics Sonochemistry* 20 (2013) 535–545.
- [18] E. Esposito, E. Menegatti, R. Cortesi, Hyaluronan-based microspheres as tools for drug delivery: a comparative study, *International Journal of Pharmaceutics* 288 (2005) 35–49.
- [19] J.C. Menéndez, A. M. Sakr, Development of metronidazole controlled release pellets in the rotary fluid-bed spray granulator, *Die Pharmazeutische Industrie* 65(5) (2003) 448-453.
- [20] N. Skalko-Basnet, Z. Pavelic, M. Becirevic-Lacan, Liposomes Containing Drug and Cyclodextrin Prepared by the One-Step Spray-Drying Method, *Drug Development and Industrial Pharmacy* 26(12) (2000) 1279–1284.
- [21] M. Szekalska, K. Winnicka, A. Czajkowska-Kosnik, K. Sosnowska, A. Amelian, Evaluation of Alginate Microspheres with Metronidazole Obtained by the Spray Drying Technique, *Acta Poloniae Pharmaceutica* 72(3) (2015) 569-578.
- [22] M. Kilicarslan, M. Gumustas, S. Yildiz, T. Baykara, Preparation and Characterization of Chitosan-Based Spray-Dried Microparticles for the Delivery of Clindamycin Phosphate to Periodontal Pockets, *Current Drug Delivery* 11(1) (2014) 98–111.
- [23] G. Perera, J. Barthelmes, A. Bernkop-Schnürch, Novel pectin–4-aminothiophenole conjugate microparticles for colon-specific drug delivery, *Journal of Controlled Release* 145(3) (2010) 240–246.
- [24] C. M. Oh, P. W. S. Heng, L. W. Chan, Influence of Hydroxypropyl Methylcellulose on Metronidazole Crystallinity in Spray-Congeaed Polyethylene Glycol Microparticles and Its Impact with Various Additives on Metronidazole Release, *AAPS PharmSciTech*, 16(6) (2015) 1357–1367.

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65
- [25] A. Paudel, Z. A. Worku, J. Meeus, S. Guns, G. V. den Mooter, Manufacturing of solid dispersions of poorly water soluble drugs by spray drying: Formulation and process considerations, *International Journal of Pharmaceutics* 453 (2013) 253– 284.
- [26] A. Singh, G. Van den Mooter, Spray drying formulation of amorphous solid dispersions, *Advanced Drug Delivery Reviews*, 100 (2016) 27-50.
- [27] P. Di Martino, R. Censi, L. Malaj, D. Capsoni, V. Massarotti, and S. Martelli, Influence of solvent and crystallization method on the crystal habit of metronidazole, *Crystal Research and Technology*, 42 (2007) 800 – 806.
- [28] C. F. Rediguieri, V. Porta, D. S. Nunes, T. M Nunes, H. E. Junginger, S. Kopp, K. K. Midha, V. P. Shah, S. Stavchansky, J. B. Dressman, D. M. Barends, Biowaiver Monographs for Immediate Release Solid Oral Dosage Forms: Metronidazole, *Journal of Pharmaceutical Sciences*, 100 (2011) 1618-27.
- [29] F. S. Aleanizy, F. Alqahtani, O. Al Gohary, E. El Tahir, R. Al Shalabi, Determination and characterization of metronidazole–kaolin interaction, *Saudi Pharmaceutical Journal*, 23(2) (2015) 167–176.
- [30] R. B. Chavan, R. Thipparaboina, D. Kumara, N. R. Shastri, Evaluation of the inhibitory potential of HPMC, PVP and HPC polymers on nucleation and crystal growth, *RSC Adv.*, 6(81) (2016) 77569–77576.
- [31] X. He, L. Pei, H. H. Y. Tong, Y. Zheng, Comparison of Spray Freeze Drying and the Solvent Evaporation Method for Preparing Solid Dispersions of Baicalein with Pluronic F68 to Improve Dissolution and Oral Bioavailability, *AAPS PharmSciTech*, 12(1) (2011)104-113.
- [32] C. Santos, C. J. Silva, Zs. Büttel, R. Guimarães, S. B. Pereira, P. Tamagnini, A. Zille, Preparation and characterization of polysaccharides/PVA blend nanofibrous membranes by electrospinning method, *Carbohydrate Polymers*, 99 (2014) 584–592.

1 [33] C. Arpagaus, P. John, A. Collenberg, D. Rütli, Nanocapsules formation by nano spray
2 drying, Nanoencapsulation Technologies for the Food and Nutraceutical Industries, (2017)
3
4 346–401.
5

6
7 [34] J. Das, M. Dhua, UV-Spectrophotometric Assay Method Development and Validation
8 of Metronidazole in Bulk and Tablet Formulation, Journal of PharmaSciTech, 3 (2) (2014) 106-
9
10 109.
11
12

13
14 [35] C. G. da Rosa, C. D. Borges, R. C. Zambiasi, M. R. Nunes, E. V. Benvenuti, S. R. da
15 Luz, R. F. D’Avila, J. K. Rutz, Microencapsulation of gallic acid in chitosan, β -cyclodextrin
16 and xanthan, Industrial Crops and Products, 46 (2013) 138-146.
17
18
19

20
21 [36] Malvern Instruments Ltd., Operators Guide, MAN 0247, Issue 2.0, Worcestershire.
22
23 WR14 1XZ, available at [Mastersizer 2000 user manual \(English\) | Malvern Panalytical](#)
24
25 (October 1999).
26
27

28
29 [37] L. Wang, A. Wang, X. Zhao, X. Liu, D. Wang, F. Sun, Y. Li, Design of a long-term
30 antipsychotic in situ forming implant and its release control method and mechanism,
31 International Journal of Pharmaceutics 427 (2012) 284– 292.
32
33
34

35
36 [38] J. Vicente, J. Pinto, J. Menezes, F. Gaspar, Fundamental analysis of particle formation
37 in spray drying, Powder Technology 247 (2013) 1–7.
38
39

40
41 [39] M. Cirri, F. Maestrelli, S. Scuota, V. Bazzucchi, P. Mura, Development and
42 microbiological evaluation of chitosan and chitosan-alginate microspheres for vaginal
43 administration of metronidazole, International Journal of Pharmaceutics 598 (2021) 120375.
44
45
46

47
48 [40] B. Davani, Metronidazole, available at
49
50 http://www.pharmacopeia.cn/v29240/usp29nf24s0_m53670.html
51
52
53
54
55
56
57
58
59
60
61
62
63
64
65

1
2
3
4
5 [41] B. T. Surikutchi, P. P. Shashank, S. Ganesh, P. Sarsvatkumar and K. B. Arvind, Drug-
6
7 excipient behavior in polymeric amorphous solid dispersions, *Journal of Excipients and Food*
8
9 *Chemicals*, 4(3) (2014) 70-94.

10
11 [42] D. J. Blundell, On the interpretation of multiple melting peaks in poly(ether ether
12
13 ketone), *POLYMER*, 28(13) (1987) 2248-2251.

14
15 [43] P. Corradini, R. Napolitano, L. Oliva, V. Petraccone, B. Piroui, A Possible Structural
16
17 Interpretation of the Two DSC Melting Peaks of Isotactic Polypropylene in the α -Modification,
18
19 *Makromol. Chem., Rapid Commun.* 3 (1982) 753–756.

20
21 [44] K. K. Nanda, Size-dependent melting of nanoparticles: Hundred years of
22
23 thermodynamic model, *Pramana*, 72(4) (2009) 617–628.

24
25 [45] S. K. Gupta, M. Talati, P. K. Jha, Shape and Size Dependent Melting Point Temperature
26
27 of Nanoparticles, *Materials Science Forum*, 570 (2008) 132–137.

28
29 [46] S. Q. Chang, Y. Wang, B. K. Tay, S. Li, H. Huang, Y. B. Zhang, Correlation between
30
31 the Melting Point of a Nanosolid and the Cohesive Energy of a Surface Atom, *J. Phys. Chem*,
32
33 106(41) (2002) 10701–10705.

34
35 [47] P. M. Shafi, A. C. Bose, Impact of crystalline defects and size on X-ray line broadening:
36
37 A phenomenological approach for tetragonal SnO₂ nanocrystals, *AIP Advances*, 5(5) (2015)
38
39 057137.

40
41 [48] A. Kaur, P. K. Parmar, A. K. Bansal, Evaluation of Different Techniques for Size
42
43 Determination of Drug Nanocrystals: A Case Study of Celecoxib Nanocrystalline Solid
44
45 Dispersion, *Pharmaceutics*, 11 (2019) 516.

46
47 [49] P. Roumanille, V. Baco-Carles, C. Bonningue, M. Gougeon, B. Duployer, P. Monfraix,
48
49 H. Le Trong, P. Tailhades, Bi₂(C₂O₄)₃·7H₂O and Bi(C₂O₄)OH Oxalates Thermal
50
51
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Decomposition Revisited. Formation of Nanoparticles with a Lower Melting Point than Bulk Bismuth, *Inorganic Chemistry*, 56(16) (2017) 9486–9496.

[50] Y. Huang, W. G. Dai, Fundamental aspects of solid dispersion technology for poorly soluble drugs, *Acta Pharmaceutica Sinica B*, 4(1) (2014) 18–25.

[51] J. Hu, Y. C. Dong, W. K. Ng, G. Pastorin, Preparation of drug nanocrystals embedded in mannitol microcrystals via liquid antisolvent precipitation followed by immediate (on-line) spray drying, *Advanced Powder Technology*, 29(4) (2018) 957-963

Metronidazol-polymer composites were prepared by nano spray drying.

In the solid dispersion metronidazol was crystalline and amorphous in polymer matrix.

Melting point decrease phenomena was observed by DSC measurement.

Peak broadening was observed by XRD analysis.

The composite microparticles were nanostructured.

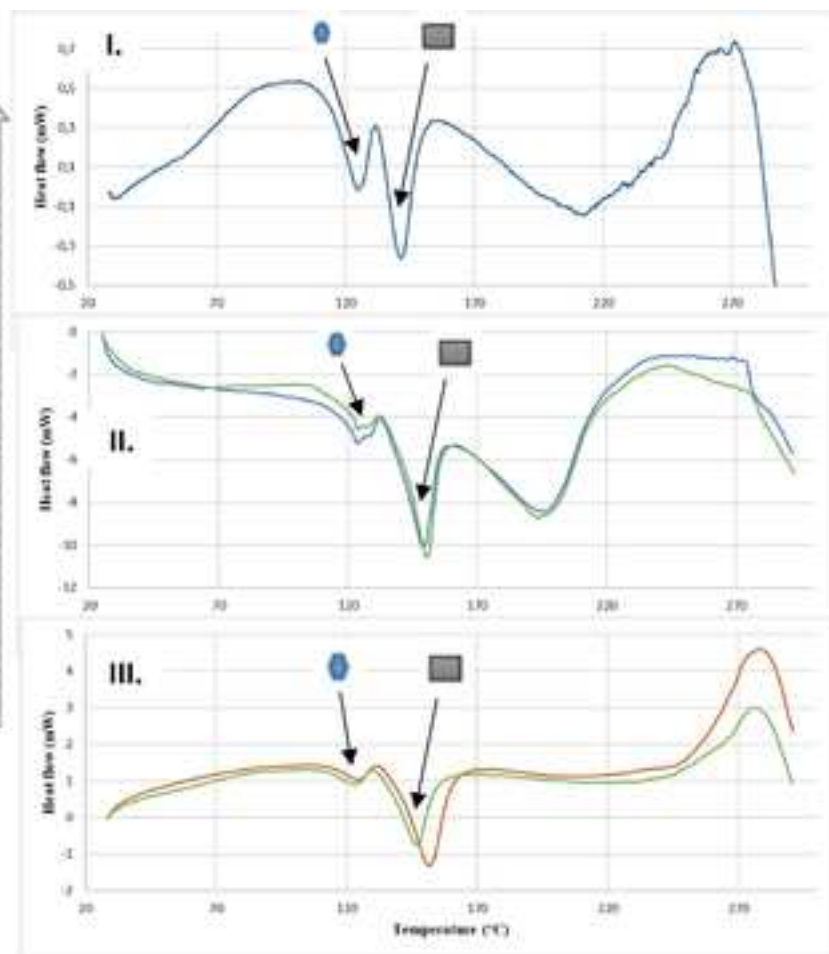
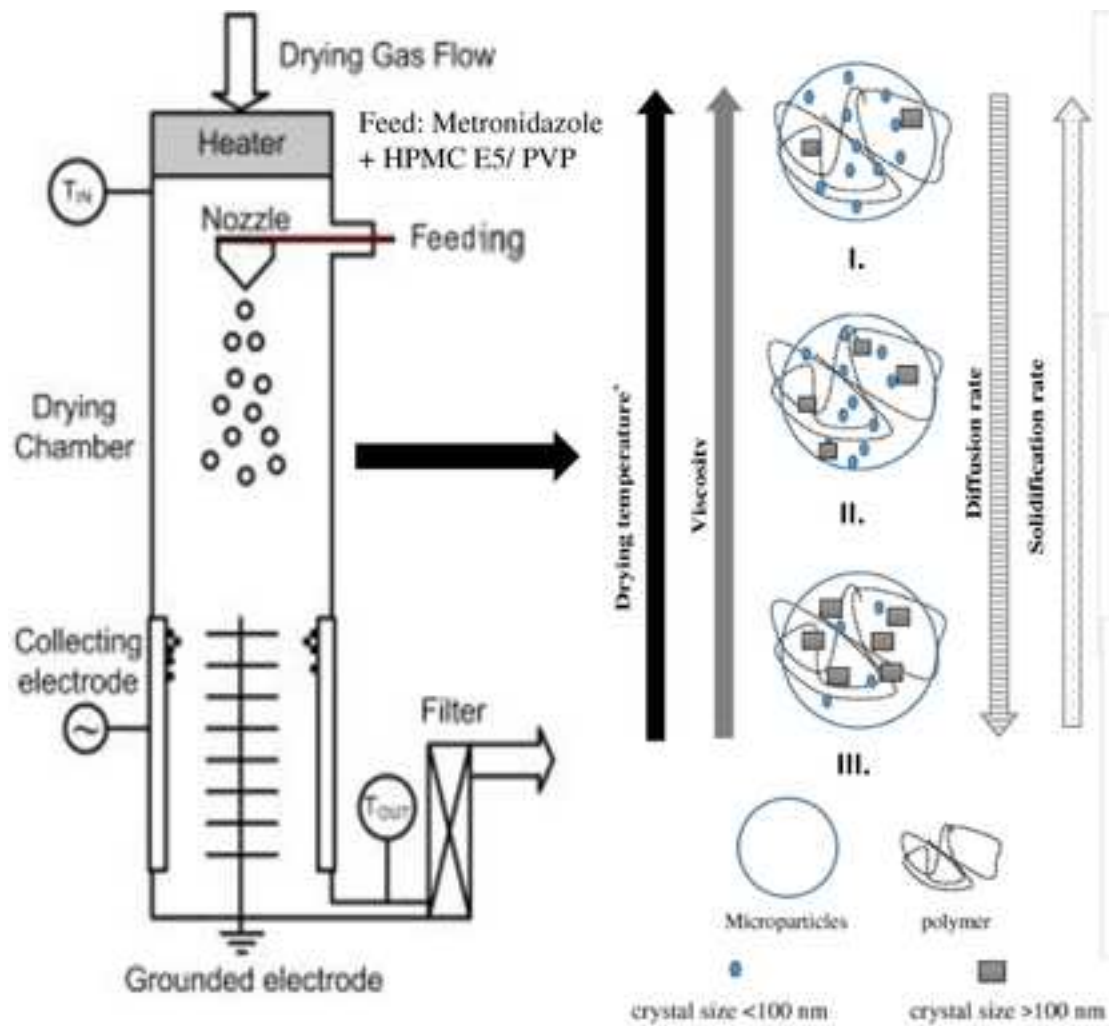


Table 1 - The main process parameters of drying experiments

| No. | $C_{MTZ,s}$ %(w/w) | C_p %(w/w) | Polymer | C_A %(w/w) | Admixture | T_{in} (° C) | Membrane size (μ m) | Spray % | V_{air} (L/min) |
|--------------------|-----------------------|-----------------|---------|-----------------|--------------|-------------------|-----------------------------|------------|----------------------|
| M | 1.0 | - | - | - | - | 120 | 5.5 | 40-70 | 90 |
| MH1 | 1.0 | 1.0 | HPMC | - | - | 110 | 7 | 55 | 90 |
| MH2 | 0.5 | 1.5 | HPMC | - | - | 120 | 7 | 60-70 | 90 |
| MH3 | 0.5 | 1.5 | HPMC | - | - | 100 | 7 | 30-50 | 90 |
| MH4 | 0.5 | 1.0 | HPMC | - | - | 120 | 7 | 30 | 120 |
| MH5 | 0.5 | 1.0 | HPMC | - | - | 120 | 7 | 30 | 100 |
| MH6 | 0.5 | 1.0 | HPMC | - | - | 120 | 7 | 30 | 90 |
| MH7 | 0.5 | 1.0 | HPMC | - | - | 100 | 7 | 30 | 120 |
| MH8 | 0.5 | 1.0 | HPMC | - | - | 100 | 7 | 30 | 90 |
| MH9 | 0.5 | 2.0 | HPMC | - | - | 120 | 7 | 60 | 90 |
| MH10 | 0.75 | 1.5 | HPMC | - | - | 100 | 7 | 50 | 90 |
| MPP1 | 0.75 | 5.0 | PVP | - | - | 100 | 7 | 30 | 90 |
| MPP2 | 0.75 | 2.5 | PVP | - | - | 100 | 7 | 30 | 90 |
| MPP3 | 0.75 | 1.5 | PVP | - | - | 100 | 7 | 30 | 90 |
| MPP4 | 0.5 | 1.5 | PVP | - | - | 100 | 7 | 30 | 90 |
| MPP2 _T | 0.75 | 2.5 | PVP | 0.1 | Tween 80 | 100 | 7 | 30 | 90 |
| MPP2 _{PA} | 0.75 | 2.5 | PVP | 0.1 | PVA | 100 | 7 | 30 | 90 |
| MPP2 _{PL} | 0.75 | 2.5 | PVP | 0.1 | Pluronic F68 | 100 | 7 | 30 | 90 |
| H | - | 1.0 | HPMC | - | - | 100 | 7 | 30 | 90 |
| PP | - | 2.5 | PVP | - | - | 100 | 7 | 30 | 90 |

$C_{MTZ,s}$: MTZ concentration in solutions to be dried, C_p : polymer concentration in solutions to be dried, C_A : admixture concentration in solutions to be dried, T_{in} : inlet temperature, V_{air} : drying air flow rate

Table 2 - Active ingredient content (C_{MTZ}), entrapment efficiency (EE%), process yield, particle size distribution (d(0.1), d(0.5), d(0.9)), volume average particle size d(4,3) of the dried products and viscosity of the solutions ($\eta_{25\text{ }^\circ\text{C}}$)

| No. | C _{MTZ} , % | EE% | Yield, (%) | d(0.1), (μm) | d(0.5), (μm) | d(0.9), (μm) | d(4,3) (μm) | $\eta_{25\text{ }^\circ\text{C}}$, mPa*s |
|--------------------|----------------------|-------|------------|---------------------------|---------------------------|---------------------------|--------------------------|---|
| M | 95.9 | - | 12.3 | | | | - | 1.05 |
| MH1 | 50.0 | 100.0 | 58.2 | 1.5 | 9.6 | 21.2 | 10.8 | 2.09 |
| MH2 | 24.3 | 97.1 | - | 2.6 | 12.7 | 26.0 | 13.9 | 2.92 |
| MH3 | 18.9 | 75.6 | 29.6 | 1.5 | 3.7 | 14.9 | 6.3 | 2.92 |
| MH4 | 18.2 | 54.6 | 47.7 | 1.5 | 5.4 | 12.7 | 6.4 | 2.07 |
| MH5 | 24.8 | 74.4 | 49.6 | 1.7 | 7.4 | 17.4 | 8.7 | 2.07 |
| MH6 | 28.4 | 85.1 | 58.4 | 2.0 | 9.4 | 20.1 | 10.4 | 2.07 |
| MH7 | 30.3 | 90.8 | 59.0 | 1.7 | 8.1 | 19.2 | 9.5 | 2.07 |
| MH8 | 29.9 | 89.8 | 63.0 | 1.9 | 9.1 | 20.2 | 10.3 | 2.07 |
| MH9 | 18.0 | 89.8 | 29.1 | 3.4 | 19.1 | 40.1 | 21.1 | 4.01 |
| MH10 | 27.4 | 82.1 | 41.3 | 1.5 | 5.1 | 13.1 | 6.4 | 2.95 |
| MPP1 | 14.5 | 111.1 | 73.1 | 1.3 | 3.8 | 11.5 | 5.3 | 2.51 |
| MPP2 | 21.2 | 91.9 | 56.6 | 1.3 | 2.8 | 5.8 | 3.4 | 1.63 |
| MPP3 | 32.7 | 98.0 | 16.9 | 4.6 | 26.0 | 114.0 | 44.7 | 1.34 |
| MPP4 | 24.2 | 96.7 | 59.7 | 1.2 | 4.5 | 13.9 | 6.3 | 1.34 |
| MPP2 _T | 22.0 | 98.3 | 55.6 | 1.4 | 8.0 | 19.5 | 9.4 | - |
| MPP2 _{PA} | 22.3 | 99.7 | 72.0 | 1.3 | 6.4 | 15.0 | 7.5 | - |
| MPP2 _{PL} | 21.6 | 96.3 | 69.3 | 1.3 | 7.5 | 16.7 | 8.3 | - |
| H | - | - | 61.3 | 1.5 | 5.0 | 15.1 | 7.6 | 2.11 |
| PP | - | - | 78.8 | 1.3 | 3.0 | 7.7 | 3.9 | 1.60 |

Table 3 - Calorimetric data of MTZ and selected dried products

| No. | C _{MTZ} , % | Onset, (°C) | Offset, (°C) | Peak 1, (°C) | Peak 2, (°C) | Total melting enthalpy (J/g) |
|--------------------|-------------------------|----------------|-----------------|-----------------|-----------------|---------------------------------|
| MTZ | 100.0 | 159.7 | 174.7 | 163.8 | - | 158.6 |
| M | 95.9 | 157.5 | 166.3 | 160.3 | - | 178.0 |
| MH1* | 50.0 | 120.1 | 159.0 | 126.3 | 154.9 | 69.1 |
| MH2* | 24.3 | 99.1 | 145.6 | 114.9 | 136.0 | 22.1 |
| MH3* | 18.9 | 111.1 | 145.3 | 124.5 | 138.3 | 18.0 |
| MH4* | 18.2 | 119.5 | 147.3 | 123.3 | 142.9 | 14.5 |
| MH5* | 24.8 | 115.5 | 153.0 | 125.1 | 146.3 | 32.6 |
| MH6* | 28.4 | 119.6 | 155.5 | 123.4 | 149.1 | 36.7 |
| MH7* | 30.3 | 108.8 | 156.1 | 123.4 | 150.4 | 38.0 |
| MH8* | 29.9 | 114.4 | 160.0 | 124.6 | 151.8 | 39.5 |
| MH9* | 18.0 | 111.4 | 148.8 | 125.0 | 141.3 | 17.4 |
| MH10* | 27.4 | 111.7 | 154.2 | 123.1 | 146.9 | 28.5 |
| MPP1** | 14.5 | - | - | - | - | - |
| MPP2** | 21.2 | - | - | - | - | - |
| MPP3 | 32.4 | 107.4 | 135.4 | 118.0 | - | 20.9 |
| MPP4 | 24.2 | 105.2 | 136.9 | 119.4 | - | 19.2 |
| MPP2 _T | 21.3 | 108.1 | 139.1 | 126.9 | - | 13.2 |
| MPP2 _{PA} | 21.7 | 111.3 | 138.1 | 127.1 | - | 14.4 |
| MPP2 _{PL} | 20.9 | 108.9 | 138.8 | 128.6 | - | 12.0 |

* For HPMC containing samples, peak 1 onset and peak 2 offset are listed in the table

** Inadequate fitting

Table 4 – Melting enthalpy values of selected experiments with HPMC polymer

| No. | 1. peak enthalpy (J/g) | 2. peak enthalpy (J/g) | 1. peak/2. peak enthalpies |
|-----|------------------------------|------------------------------|-------------------------------|
| MH9 | 7.3 | 10.1 | 0.72 |
| MH4 | 5.9 | 8.6 | 0.69 |
| MH5 | 11.9 | 20.7 | 0.57 |
| MH6 | 8.0 | 28.6 | 0.28 |
| MH7 | 8.2 | 29.8 | 0.28 |
| MH8 | 3.9 | 35.6 | 0.11 |
| MH1 | 1.5 | 67.6 | 0.02 |

Table 5 – Degree of crystallinity of the dried samples

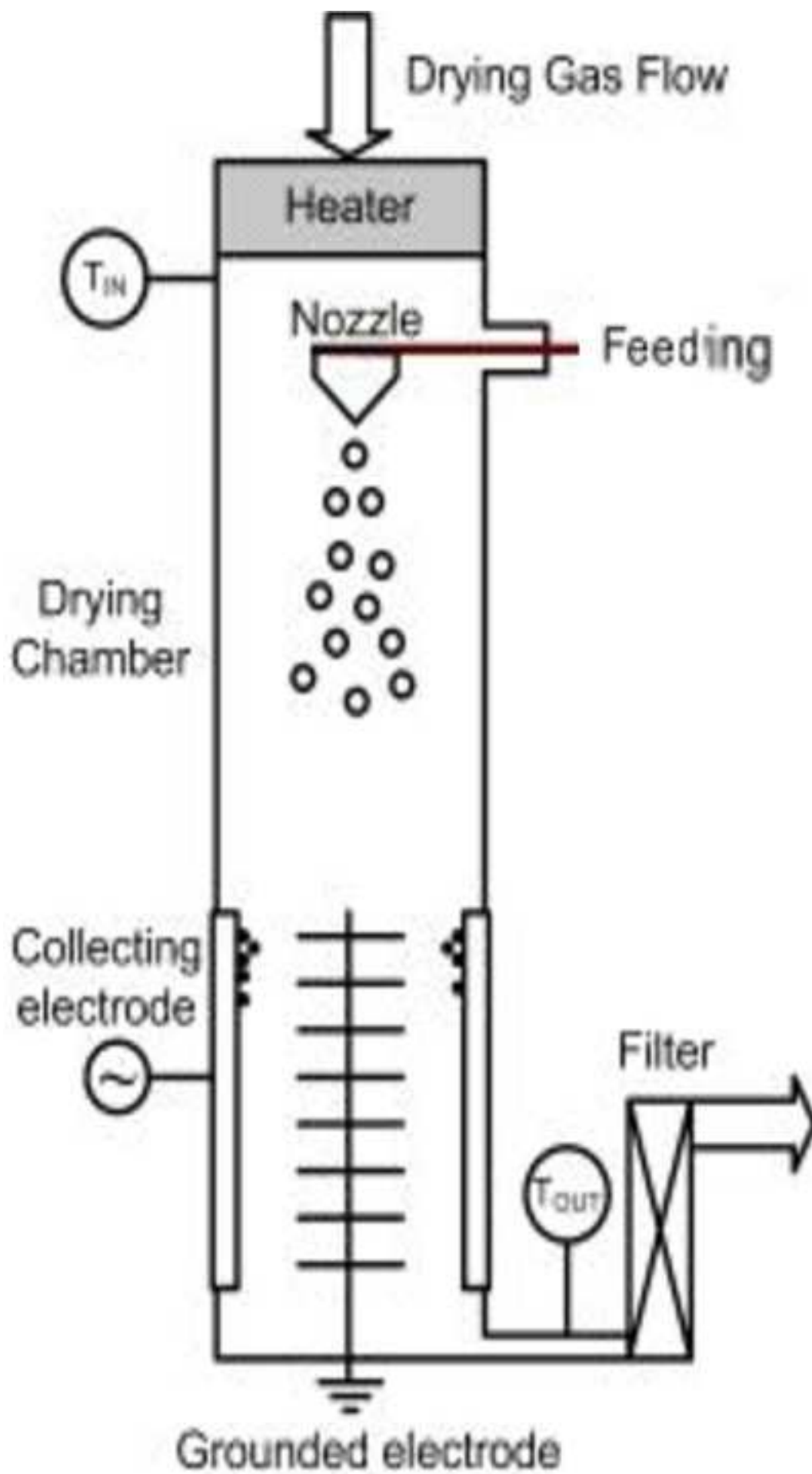
| No. | Degree of crystallinity (%) | Degree of crystallinity / MTZ content (%) |
|--------------------|-----------------------------|---|
| MTZ | 100.0 | 100.0 |
| MH1 | 43.6 | 87.1 |
| MH2 | 13.9 | 57.3 |
| MH3 | 11.4 | 60.2 |
| MH4 | 9.1 | 50.2 |
| MH5 | 20.6 | 83.0 |
| MH6 | 23.1 | 81.4 |
| MH7 | 24.0 | 79.2 |
| MH8 | 24.9 | 83.4 |
| MH9 | 11.0 | 61.0 |
| MH10 | 17.9 | 65.5 |
| MPP1* | - | - |
| MPP2* | - | - |
| MPP3 | 13.2 | 40.3 |
| MPP4 | 12.1 | 50.0 |
| MPP2 _T | 8.3 | 37.8 |
| MPP2 _{PA} | 9.0 | 40.6 |
| MPP2 _{PL} | 7.6 | 35.0 |

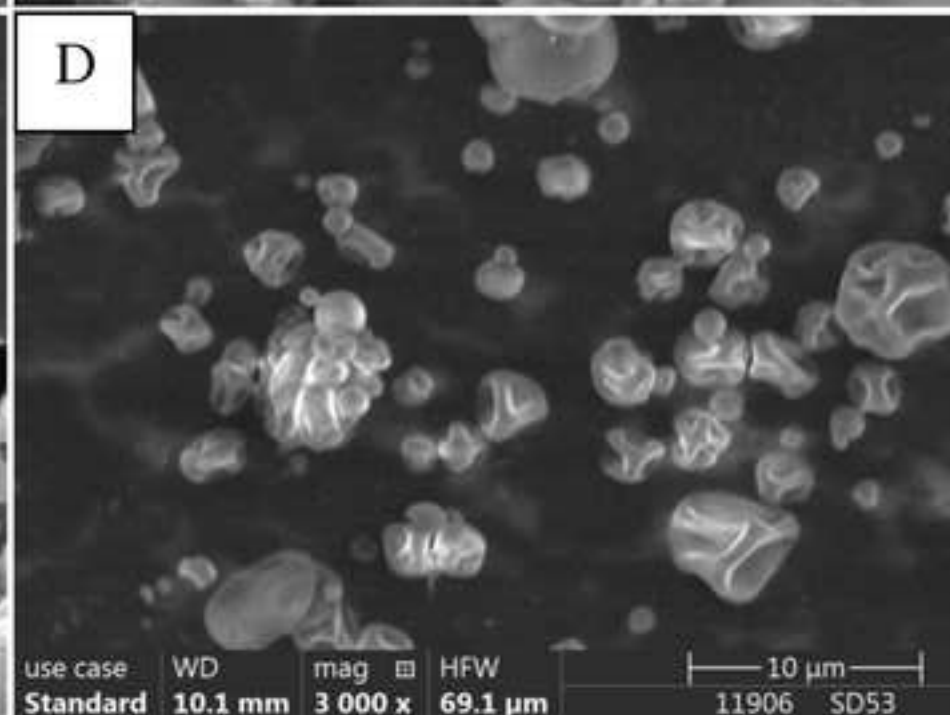
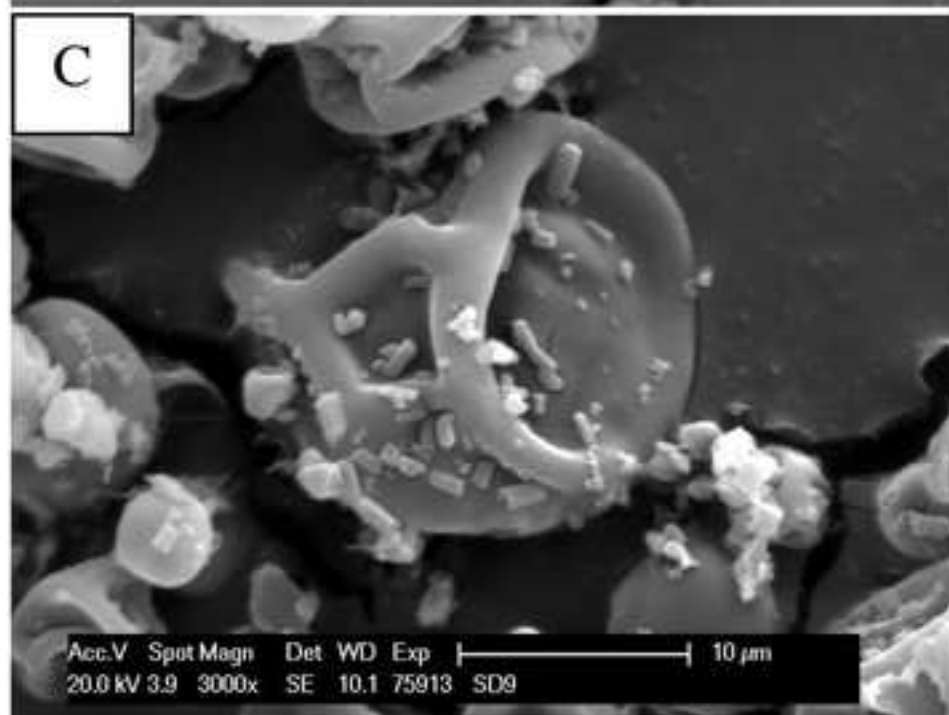
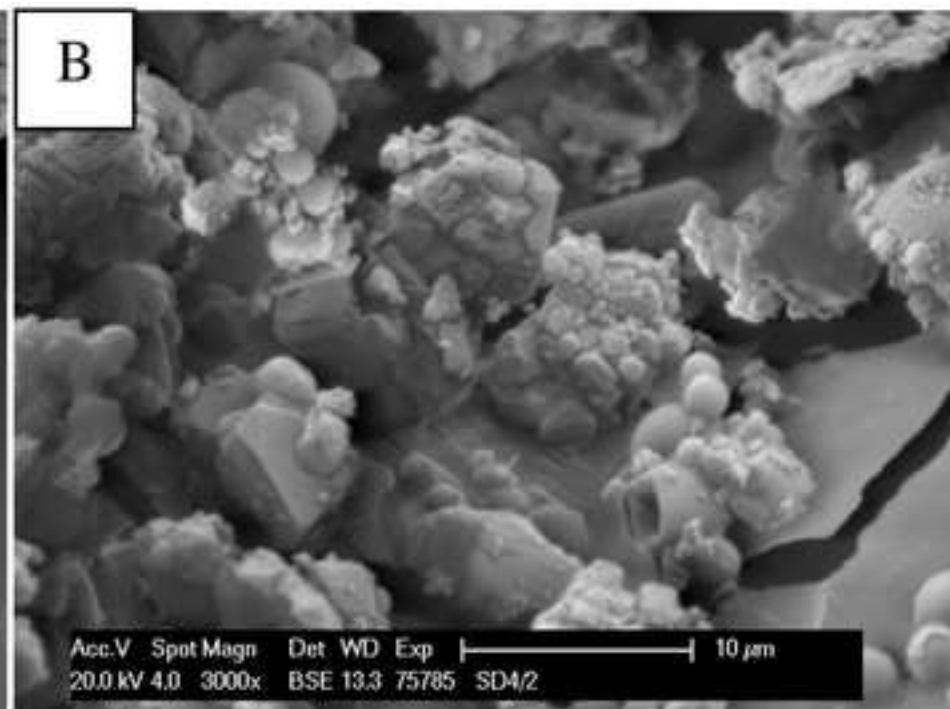
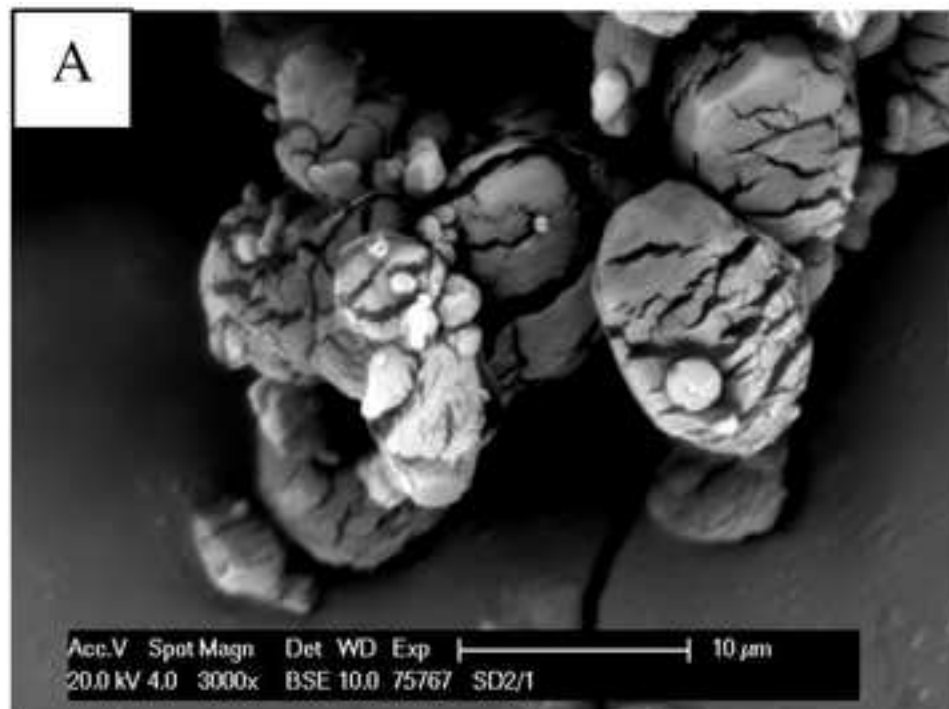
*Inadequate fitting

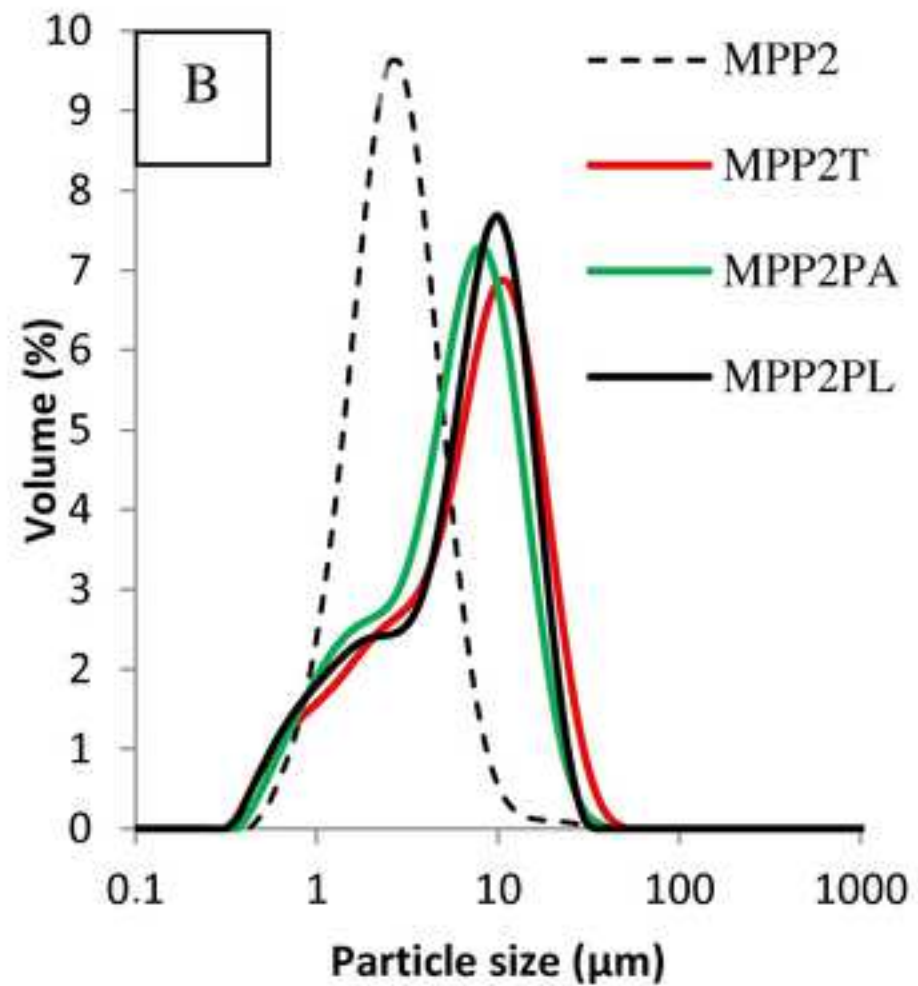
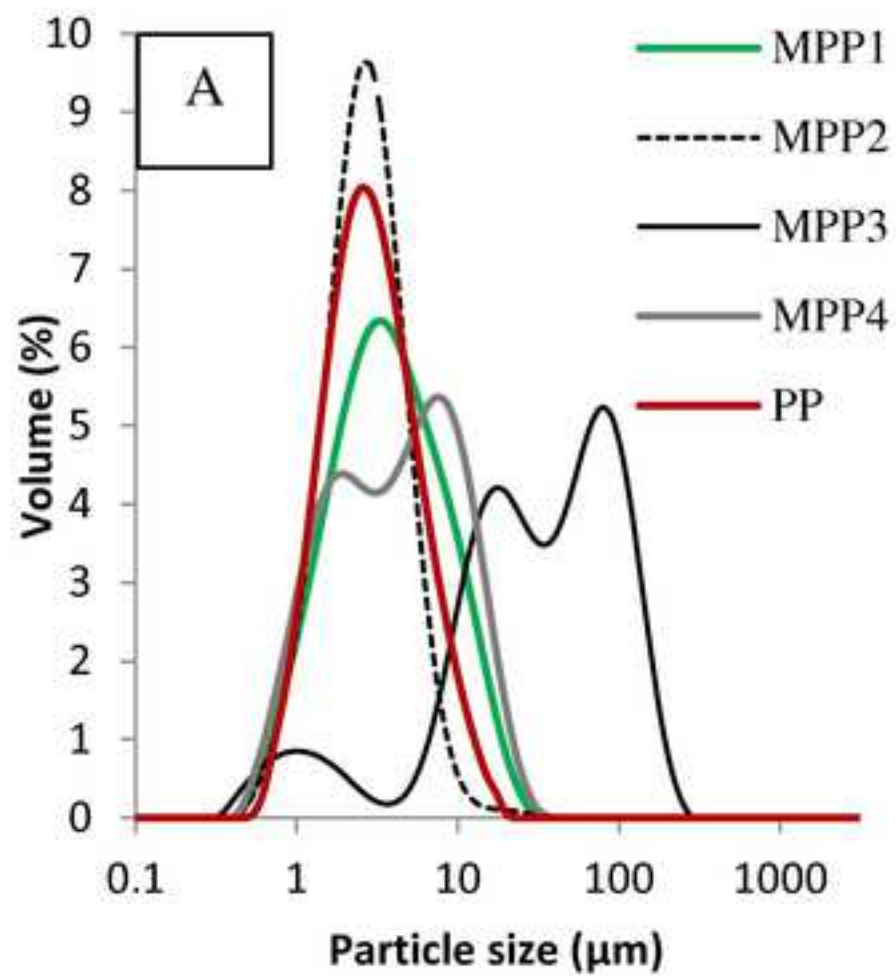
Table 6 – Selected X-ray data of samples with HPMC and PVP polymer

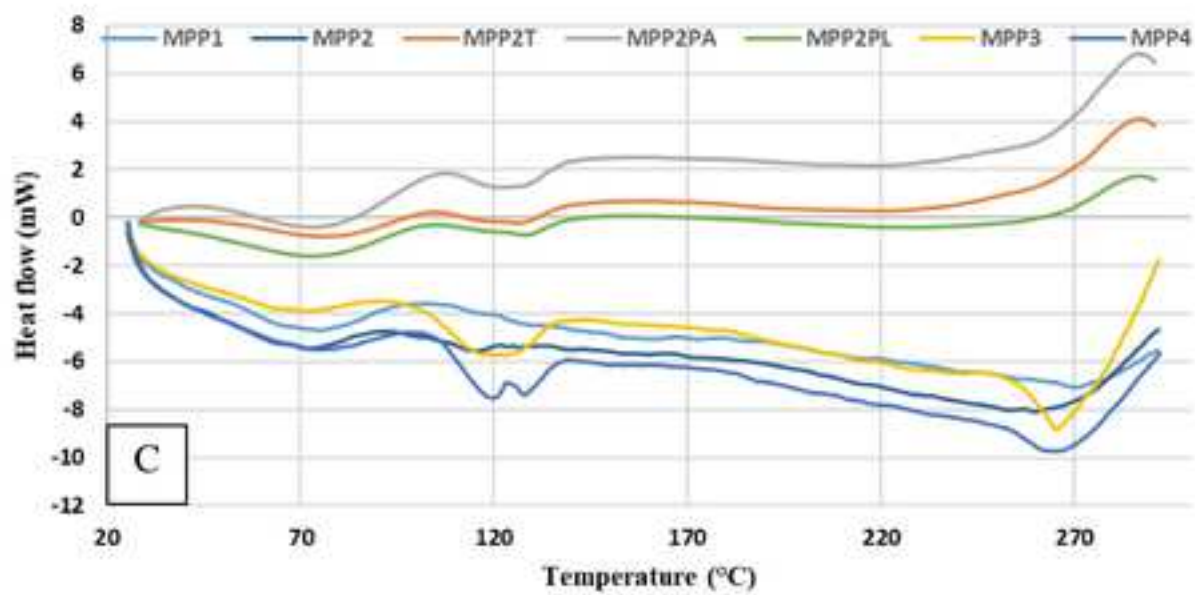
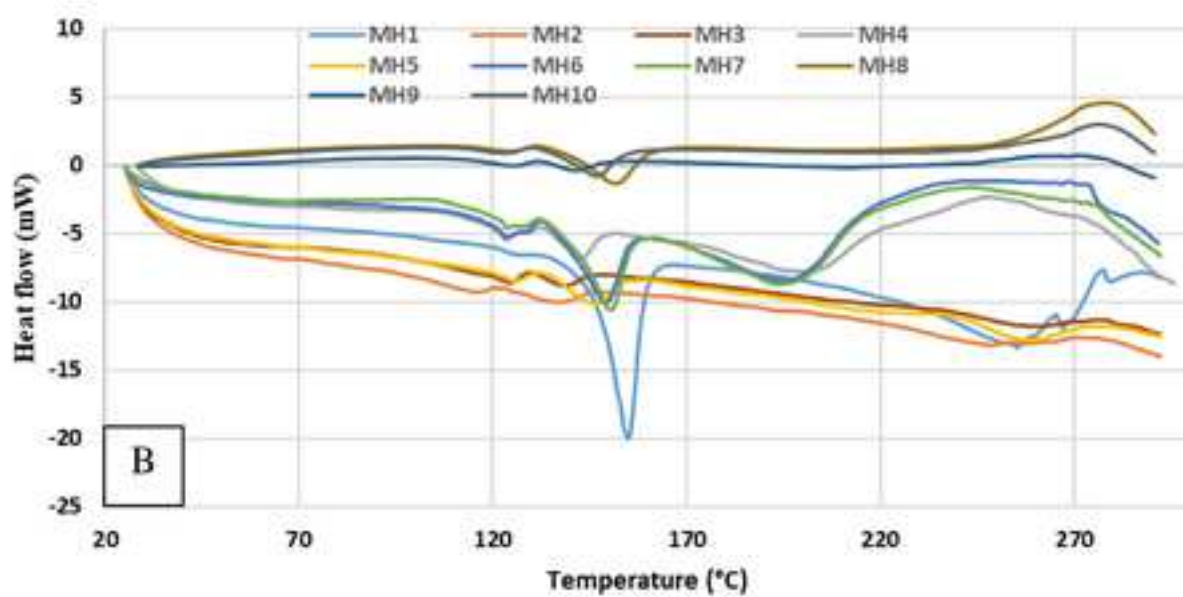
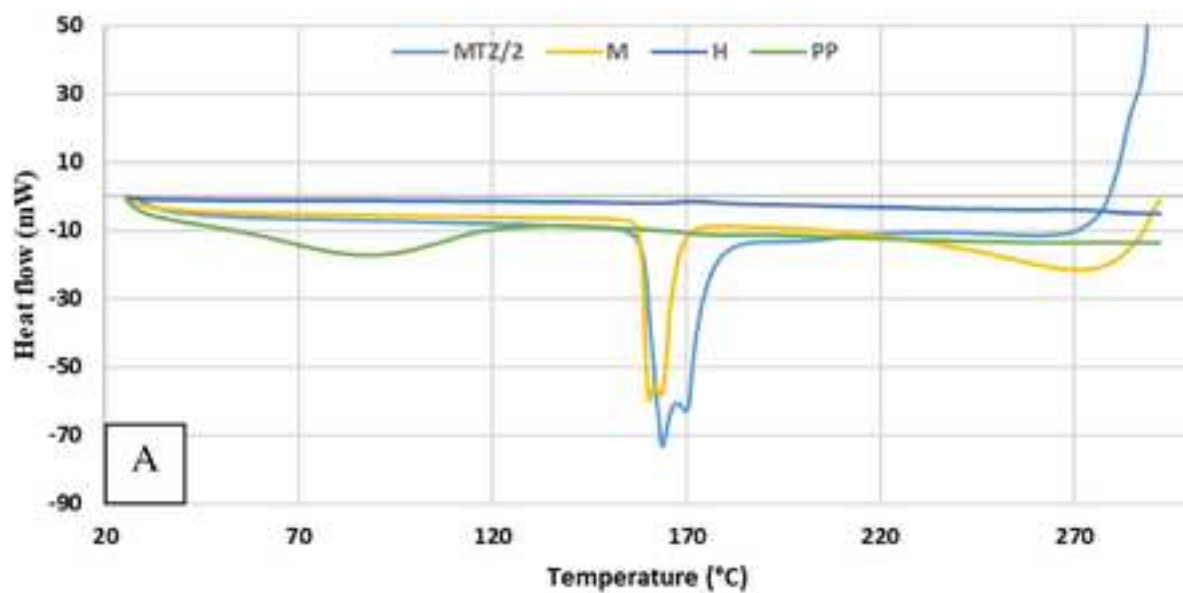
| No. | 2 θ ($^{\circ}$) | FWHM* ($^{\circ}$) | Domain size (\AA) | 2 θ ($^{\circ}$) | FWHM* ($^{\circ}$) | Domain size (\AA) | 2 θ ($^{\circ}$) | FWHM* ($^{\circ}$) | Domain size (\AA) |
|------|------------------------------|-------------------------|---------------------------------|------------------------------|-------------------------|---------------------------------|------------------------------|-------------------------|---------------------------------|
| MTZ | 12.081 | 0.103 | | 13.601 | 0.166 | | 32.979 | 0.189 | |
| MH6 | 11.994 | 0.264 | 496 | 13.552 | 0.311 | 552 | 32.950 | 0.620 | 192 |
| MH7 | 12.042 | 0.291 | 425 | 13.609 | 0.327 | 497 | 33.068 | 0.388 | 416 |
| MH9 | 11.976 | 0.326 | 358 | 13.553 | 0.319 | 523 | 33.022 | 0.346 | 528 |
| MPP4 | 12.019 | 0.243 | 571 | 13.584 | 0.258 | 870 | 33.014 | 0.558 | 225 |

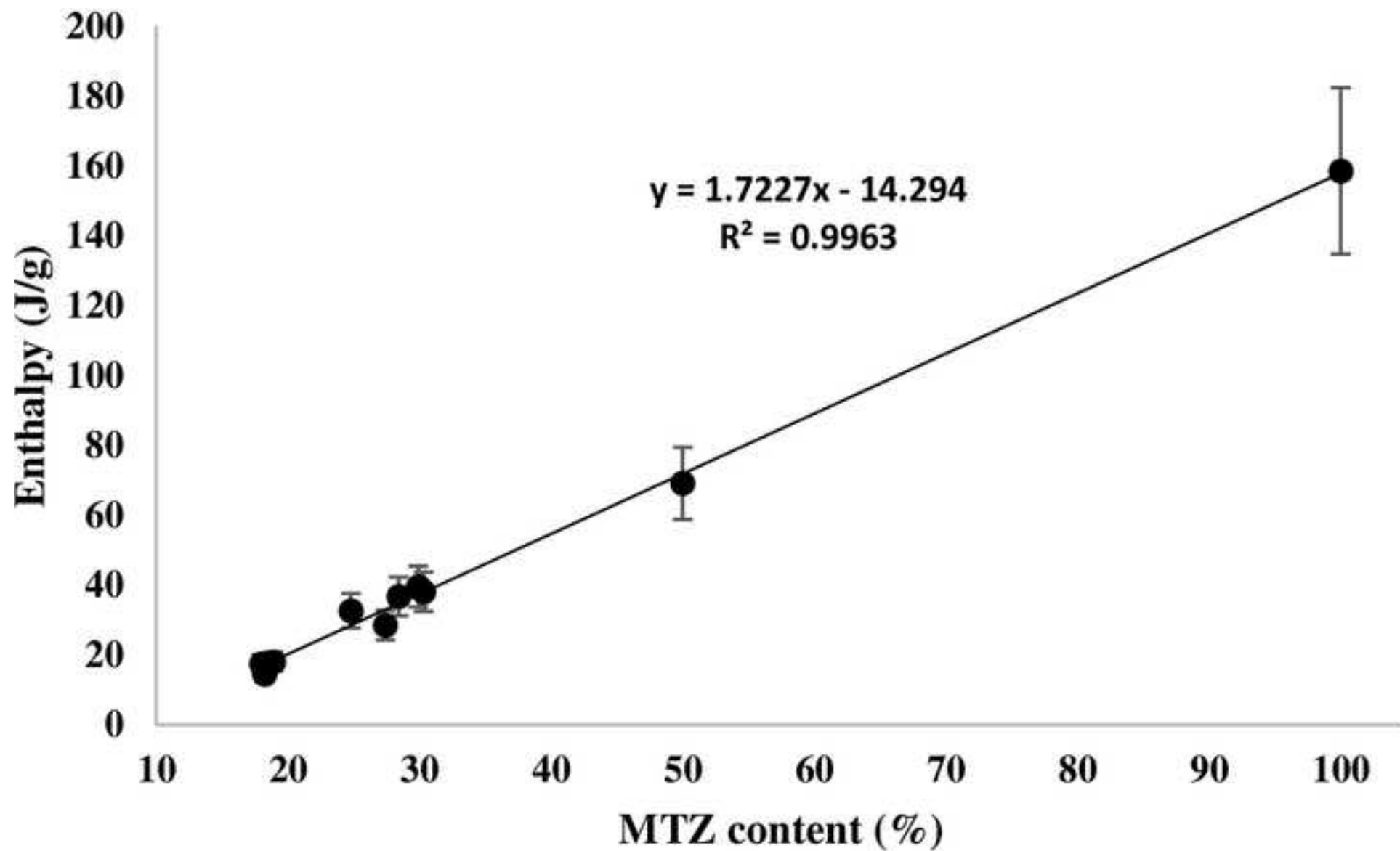
*FWHM: full width at half maximum

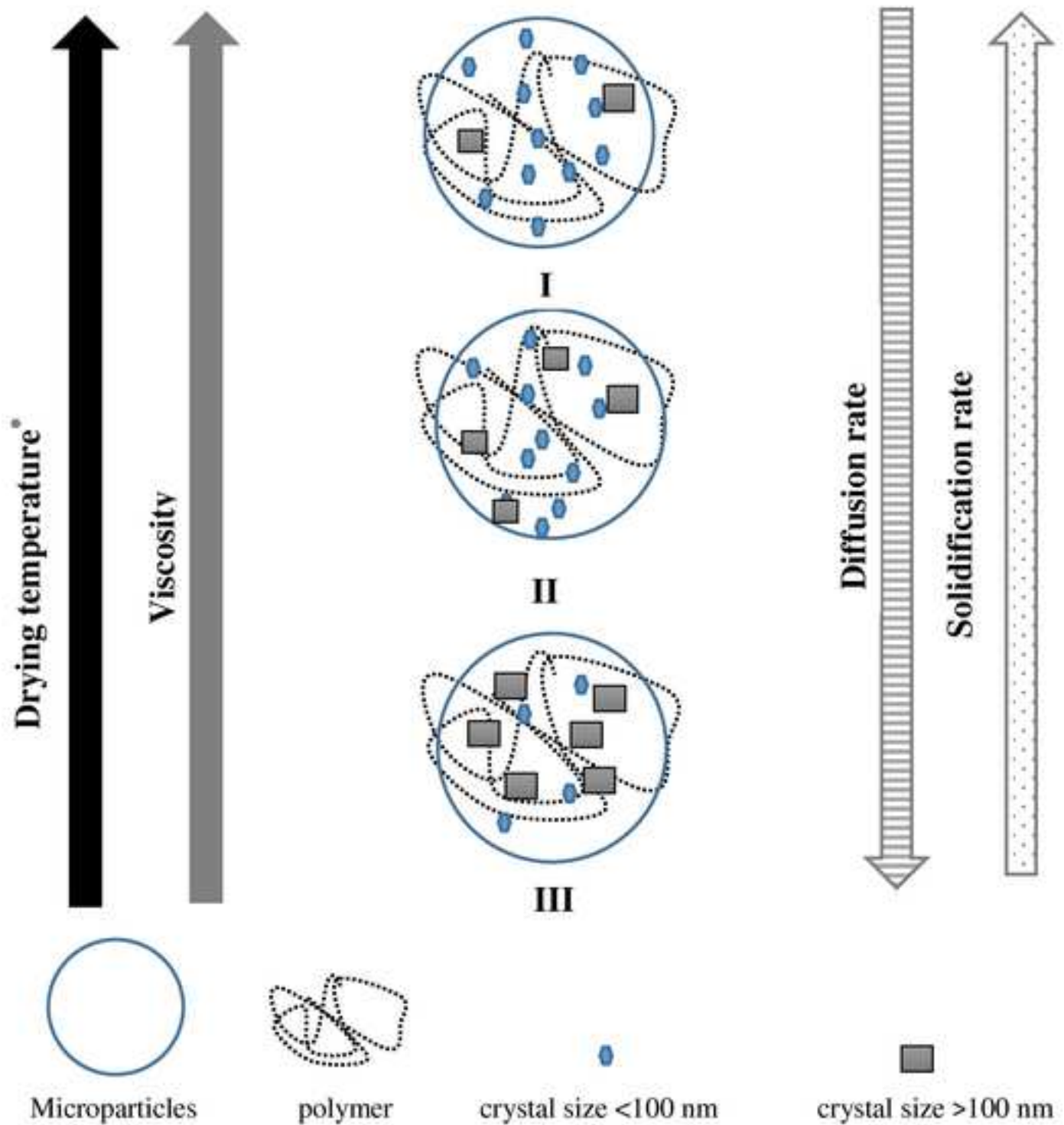










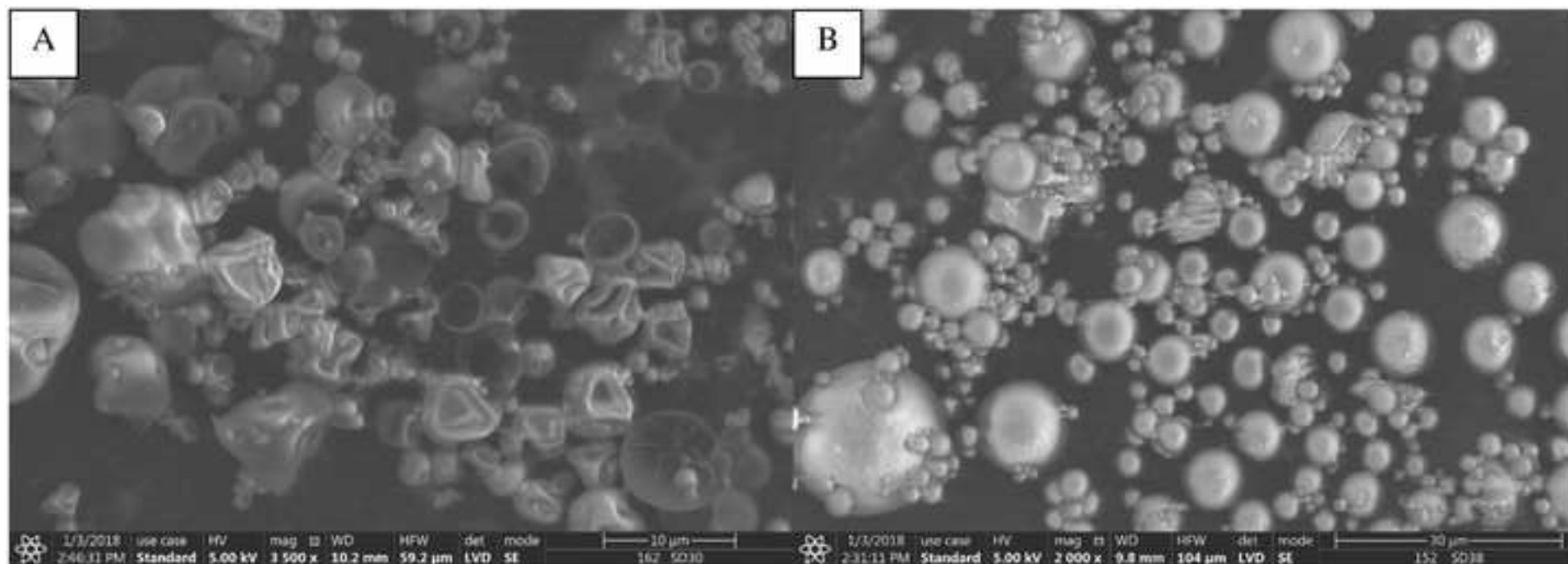


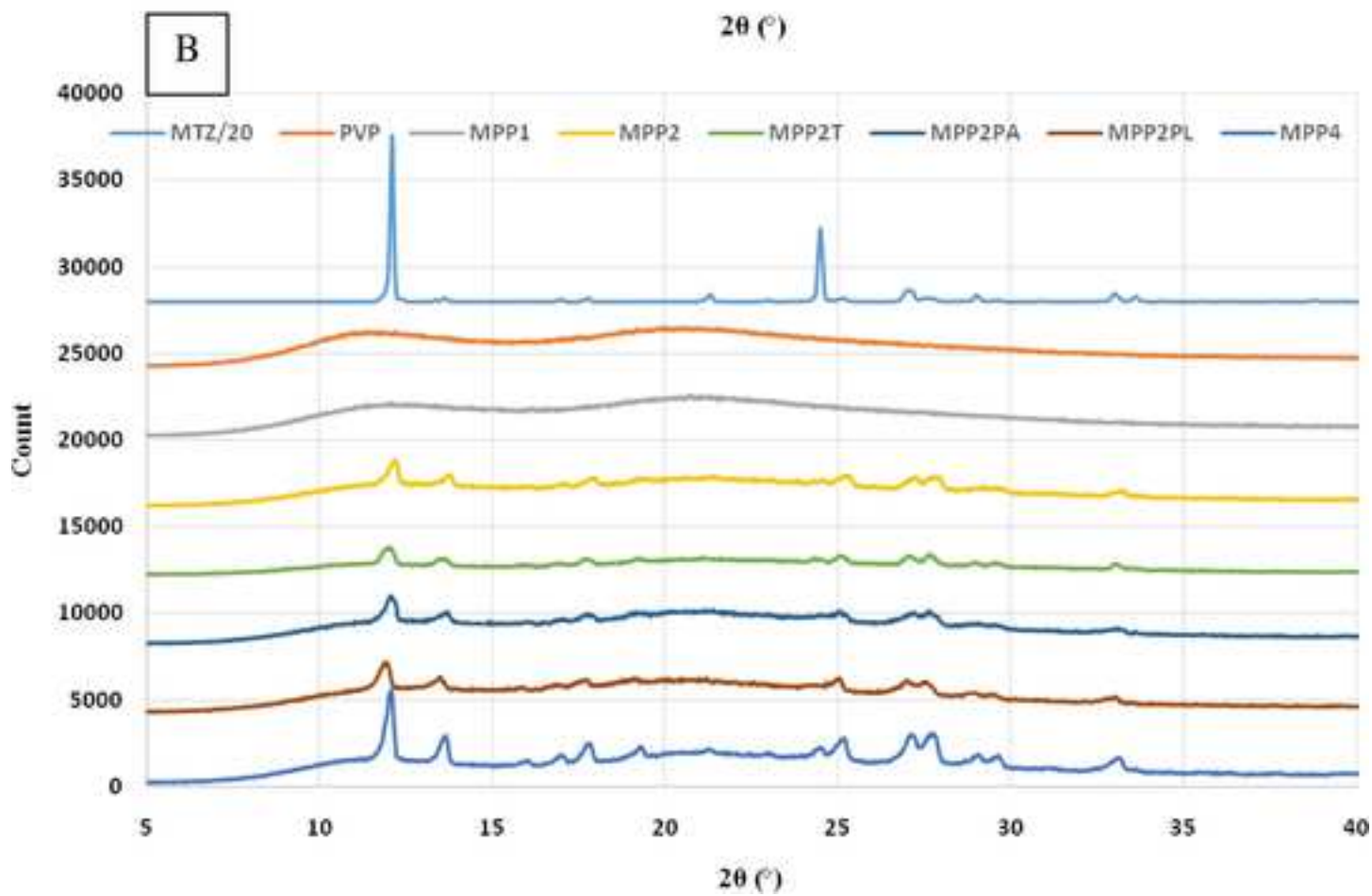
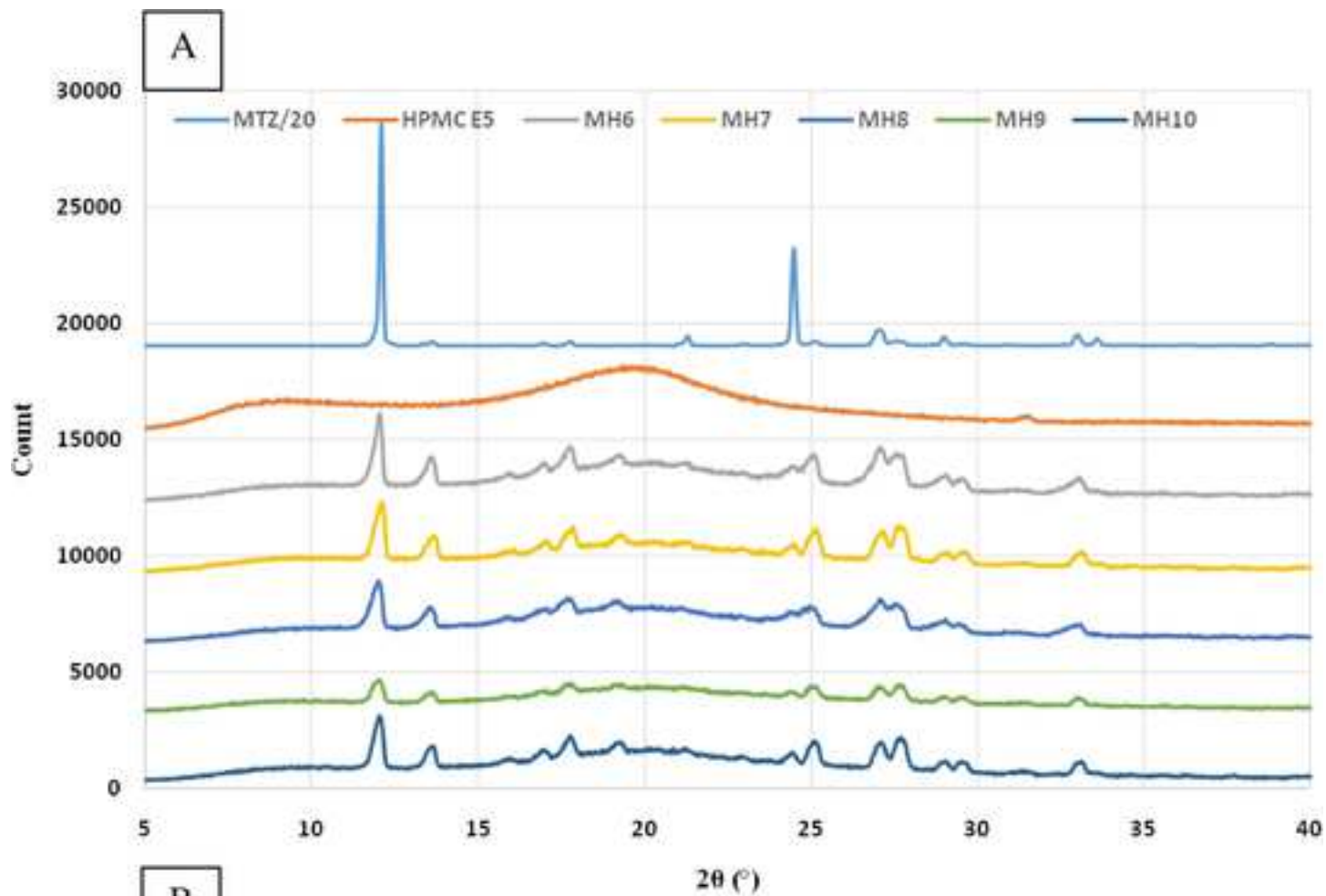
I: high drying temperature and/or high viscosity (MH4, MH9)

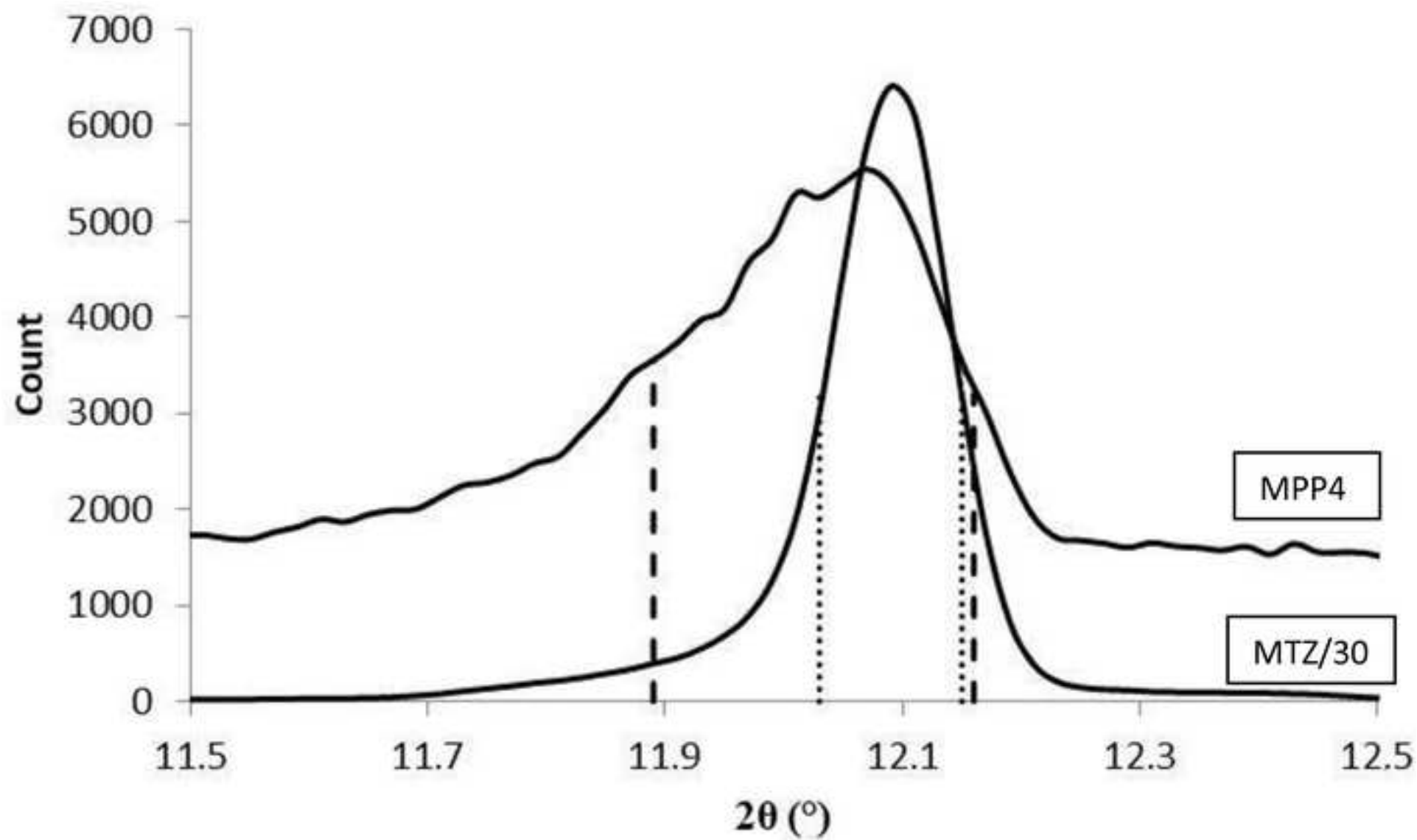
II: medium drying temperature and/or medium viscosity (MH6, MH7)

III: low drying temperature and/or low viscosity (MH10, MH8)

*drying temperature is determined by the inlet temperature and air flow rate







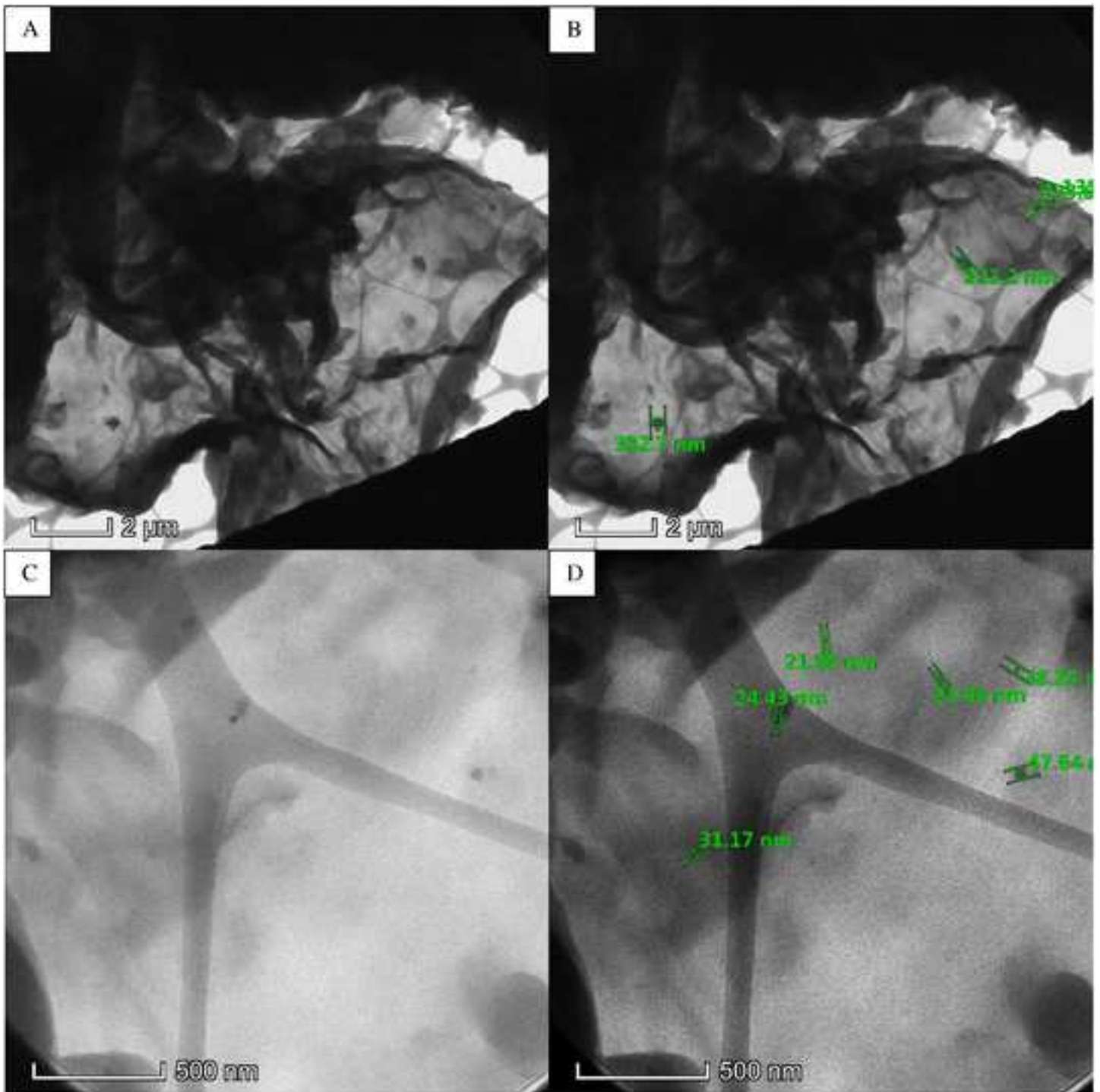


Fig. 1 Schematic set-up of the Büchi Nano Spray Dryer B-90

Fig. 2 SEM images of samples M (A), MH1 (B), MH2 (C) and MH3 (D)

Fig. 3 Particle size distributions of dried products with PVP (A) and PVP with different admixtures (B)

Fig. 4 DSC curves for MTZ (the values of heat flow of MTZ were divided by 2), M, H and PP (A), samples with HPMC (B) and PVP (C) polymers

Fig. 5 Total melting enthalpy vs. active ingredient content of samples with HPMC polymer (error bar 15%)

Fig. 6 Crystal formation during spray drying with dependency of crystal size on formulation variables and diffusion and solidification rates

Fig. 7 Particle shape of experiments with different polymers HPMC (MH4) (A) and PVP (MPP1) (B)

Fig. 8 X-ray curves of experiments with HPMC (A) and PVP (B) polymers (the counts of MTZ were divided by 20)

Fig. 9 Peak broadening of experiment MPP4 comparing to MTZ (the counts of MTZ were divided by 30), the FWHM is signed

Fig. 10 TEM images of run MH2 in two different magnification (lowest A and B, highest C and D)