

Heart performance of lambs and its relation to muscle volume and body surface

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8 **Abstract**

9 ECG gated dynamic magnetic resonance imaging (MRI) methodology was developed for in
10 vivo examination of the sheep heart characteristics combining non- invasive determination
11 of skeletal muscle mass, to study the relationship between total body skeletal muscle
12 content and heart performance. Measurements were carried out in merino type male lambs
13 using a 1.5 T field-strength equipment. During post processing of the images average left
14 ventricular volumes were determined and stroke volume (SV) was estimated. Ejection
15 fraction was calculated ($73 \pm 1.8\%$) and the cardiac output (CO) value was estimated (2.75
16 ± 0.16 L/min). After measuring left ventricular wall thickness, contraction values were
17 determined at the septum (62%), at the anterior (69%), the lateral (54 %) and the posterior
18 (58%) walls and the ventricular mass were calculated. Immediately after the MRI
19 examination, body composition measurement was performed by computerized tomography
20 (CT) during the same narcosis. From the interpretation of the functional MRI and

21 volumetric CT results, relative CO value was developed, expressing the relationship
22 between heart performance and total body skeletal muscle volume. Finally, CO value
23 related to body surface was estimated ($18.3 \pm 3.1 \text{ dm}^2/(\text{L} * \text{min}^{-1})$) to characterize the
24 metabolic rate.

25

26 **Key words:** Lamb, Magnetic Resonance Imaging, Computerized Tomography, Cardiac
27 performance

28

29 **1. Introduction**

30

31 The use of electromagnetic waves is gaining more and more space in different areas of
32 animal sciences from meat quality determination (1,2) to in vivo evaluation of body
33 composition applied as a possible mean for genetic improvement of a wide variety of
34 species (3-5).

35

36 Moreover, using animal models (mouse, rat, rabbit, canine, swine, and sheep) in human
37 cardiac research give invaluable opportunity to develop new diagnostic and therapeutic
38 methods (6,7).

39 Magnetic resonance imaging (MRI) was firstly utilized as an in vivo technique for the
40 determination of body composition of animals by Kallweit et al. (1994). A study in sheep
41 indicates that the quantification of lean and fat tissue by means of prediction equations is
42 highly accurate (9). The description of the ECG-gated MRI for the in vivo measurement of
43 heart performance in pigs has been presented by Petrásí et al. (2001), and an ovine medical
44 model was first published by Pilla et al. (2003). Recently the sheep is used as a model of

45 cardiac MR imaging of different heart failures such dilated cardiomyopathy based on
46 T1mapping sequence (12). In an ovine model end-systolic volume were measured after
47 myocardial infarction with and without micro pump based partial mechanical circulatory
48 support using MRI method (13). The cardiac MRI method, together with computerized
49 tomography (CT) was applied to measure the functional heart performance of the pig and
50 heavy type turkey, in connection with body tissue composition determination (14,15). In
51 addition, as a further quantitative method for the determination of ovine cardiac
52 characteristics the real-time 3D echocardiography, as applied by Schmidt et al. (2001), also
53 may provide opportunity (16). Moreover, Segers et al. (2001) developed an indirect
54 prediction method for the heart performance characterization of sheep (17).

55 The results achieved in intensive pigs and turkeys indicate disadvantageous changes in
56 heart performance caused by the continuous selection for increasing skeletal muscle
57 volume. From this aspect the sheep seems to be less affected at present however the
58 situation may change in the future if selection for increased muscle building capacity
59 continues.

60

61 The goal of this experiment was to develop an appropriate in vivo method for the
62 quantitative measurement of the sheep heart performance and to determine basic heart
63 performance data jointly with skeletal muscle volume and body surface estimation.

64

65 **2. Materials and methods**

66

67 Methodological measurements were carried out on three merino type male lambs at the live
68 weight of 20 kg (60 ± 4 days of age). Investigations were performed at the Health Center of
69 Kaposvár University using its Siemens Magnetom Vision Plus type, magnetic resonance
70 tomograph equipment of 1.5 T magnetic field-strength and a Siemens Somatom S40 spiral

71 CT scanner. The lambs were pre medicated intramuscularly with Rometar (Xylazin 2%)
72 (Spofa; 0.2 mg/body weight kg). Following inhalation anesthesia was introduced through a
73 narcotic mask, using 3 vol% Isoflurane (Abbott Lab.) until reaching the total relaxation,
74 when the animals were intubated, and attached to a narcotic unit (Penlon evaporator,
75 Ohmeda flow-meter). Continuous deep narcosis was obtained using 1.5-2 vol% Isoflurane
76 and 2 vol% oxygen as carrier gas, similarly to the recommendation of Hikasa et al. (2000).

77

78 The MR examination was conducted using ECG-gated sequences (19). To obtain the proper
79 signal strength from the electrocardiograph, a special active electrode (Bruker Medical) was
80 used. The electrode attached to the signal cable was fixed 10 cm from the sternum, left,
81 between the third and sixth ribs, the other two directed to the left olecranon between the
82 third and sixth ribs. During the imaging process the animals were placed into a MR
83 compatible special plastic container into ventral position with extended limbs and were
84 fixed with belts. At first, quick images were taken to locate the heart according to the co-
85 ordinate system of the body. Following in the sagittal, coronal and transversal planes
86 localization images were taken to allocate the longitudinal axis of the heart. Then multislice
87 - multiphase images were taken orthogonal to the longitudinal axis of the heart from the
88 apex to the base, performing prospective data acquisition (10). The total data acquisition
89 took ca. 10-12 minutes. Altogether 9 slices and in each slice 9 images (phase) were
90 acquired according to one heart cycle (singleslice - multiphase). From the 9 transversal
91 slices representing the total heart volume 6 covered the ventricles. The phases applied were
92 characterized by the following data: echo time: 6.8 ms, repetition time: 60.0 ms, θ : 30°,
93 field of view: 400-500 mm, matrix size: 256×256 pixels, slice thickness: 8 mm, slice gap: 1

94 mm. Moreover, the left ventricular volumes were measured and the stroke volume (SV)
95 was also computed as the difference between the end-diastolic and end-systolic data. The
96 calculated ejection fraction (EF) is given as the percentage of the ratio of the SV to end-
97 diastolic volume. The left ventricular mass was calculated from the regions epicardium –
98 endocardium + papillary 1 + papillary 2 (marked in Figure 3.) times 1.05 (g/cm³). The
99 cardiac output (CO) value was estimated as a product of the SV and heart rate. The wall
100 thickness was measured by the septum, and by the anterior, lateral and posterior walls, 9
101 mm beneath the atrioventricular valve. Images were evaluated using the software MASS
102 4.1 (20).

103

104 Serial CT images were taken continuously from the neck (atlas) until the hock with 10 mm
105 slice thickness. The total body skeletal muscle volume and the body surface were
106 measured. The image analysis performed is described in detail by Romvári et al. (2004).

107

108 **3. Results**

109

110 The heart rate was monitored before and during the MRI examination. The pulse registered
111 during the total time was that according to the relaxed state (89±3 b/min). The
112 electrocardiogram attained from the foregoing time of examination gave accurate
113 information about the overall conditions and the anesthetic possibilities concerning each
114 animal.

115 The MR examination was conducted using ECG-gated sequences. Dynamic images were
116 taken orthogonal to the longitudinal heart axis, leading from the apex to the base, covering
117 all ventricles and atria, performing prospective data acquisition (Figure 1).

118 *Figure 1*

119

120 In Figure 2 six multislice-multiphase images are shown between the end diastolic- and the
121 end systolic phase.

122 *Figure 2*

123 During the post processing of the MR images the contour of the ventricular epicardium and
124 endocardium, the outline of the left ventricular papillaries was defined (Figure 3).

Figure 3 125

126 The changes of volumetric and wall thickness data of the heart cycle in time are depicted in
127 Figure 4.

Figure 4 128

129 The first phase is synchronic with the ECG R-wave, being the beginning of the isometric
130 contraction. Ventricular volume is at the maximum at this point. As the ventricular diastole
131 ends (5th to 6th phase), the phase of isometric relaxation begins. From methodological
132 point of view to characterize the heart function, it is not necessary to follow the whole heart
133 cycle, covering the phase from the end-diastole to the end-systole is sufficient.

134

135 Characteristic data concerning lamb heart performance shown in Table 1 are mean values
136 determined during the heart cycle.

137

138 Immediately after the MRI examination of the lambs, CT scanning was performed during
139 the same narcosis. First the total body muscle volume, than the body surface was measured
140 from the consecutive cross-sectional images. Resulting from the joint interpretation of MRI
141 and CT data the CO related to body surface value ($\text{dm}^2 / (\text{L} * \text{min}^{-1})$) was estimated and the
142 so called relative CO value (expressing the relationship between heart performance and
143 skeletal muscle volume in sedentary conditions ($\text{dm}^3 / (\text{L} * \text{min}^{-1})$)) was developed (Table 2).

Table 2
144

145 **4. Discussion**

146

147 When comparing our results with available data from the literature results obtained by
148 echocardiography also have to be considered taking the paucity of such results into account.
149 However it must be stressed that no echocardiography based cardiac data of sheep with
150 normal physiological state are available in the literature. The accessible data concerning in
151 vivo model arise from experiments aiming medical purposes where surgically operated
152 animals were used. Findings of Qin et al. (2000) are originated exactly from that kind of
153 experiment. They found that the LVEDV, LVESV and LVSV values were 65 ± 24 , 30 ± 11
154 and 35 ± 11 ml respectively in case of sheep's with an average body weight of 40 kg (21).
155 It was concluded also by them that the accuracy of the method can be verified by cardiac
156 MR imaging as the gold standard method. Slightly higher LVESV (37.1 ± 8.8 ml) was
157 measured and a CO value of 3.8 L/min (± 0.6) was estimated by Psaltis et al. (2008)
158 applying cardiac MRI on merino sheep (51 ± 8.1 kg) (22). These results are in good
159 accordance with our data taken the live weight difference (20 vs. 40 kg) into account.

160

161 The average 73 % ejection fraction value is remarkably higher than the corresponding data
162 of the Mangalica pig (57%), the intensive meat type pig (53%) (14) or the giant turkey
163 (51%) (15). Lower ejection fraction refers to unfavorable hemodynamic characteristics of

164 the heart. The contraction values (septal, anterior, lateral and posterior: 62%, 69%, 54% and
165 58%, respectively) calculated from the measured wall thickness data are characteristic to
166 the condition of the myocardium. Cardiomyopathy or local circulatory failures cause a
167 functional anomaly of muscle fibers, and decrease the contraction values. The deviation
168 from normal in case of the ventricular volume and contraction data is of high diagnostic
169 value.

170

171 The average heart rate of 89 bpm can be interpreted as a normal physiological condition
172 (23). The estimated CO value – arising of the stroke volume and heart rate - is one of the
173 most important measures of heart performance in human medical practice. In a sedentary
174 state, some 16 % of the cardiac output is needed to supply the skeletal musculature in
175 humans (24). According to Meyns et al. (2000), the perfusion of the sheep muscle is 6 ± 3
176 ml/g of tissue (25). Considering the measured average of 6.4 dm^3 muscle tissue and the
177 estimated 2.75 L/min CO value, altogether 14% of the total CO supplies the musculature of
178 the examined lambs under narcosis. The estimated CO value is in good accordance with the
179 corresponding data (3.4 L/min) of Geens et al. (13). Cardiac output redistribution was
180 studied in a basic experiment carried out by Hales et al. (1984) on a merino model (26).
181 According the authors the competition between skin and muscle for blood flow during
182 exercise results a lower skin perfusion which could be critical in case of heat stress.

183

184 In the human medicine the cardiac output value related to body surface is widely used to
185 characterize the metabolic rate. In our study the respective data were $18.4 \text{ dm}^2 / (\text{L} * \text{min}^{-1})$

186 which is considerably lower than the corresponding value of the BUT Big 6 turkey at the
187 same 20 kg live weight (15).

188

189 The developed “relative cardiac output value” expresses the relationship between the lamb
190 heart performance and skeletal muscle volume in sedentary conditions. In general, the
191 physical load and/or stress-induced movements of animals lead to significant changes of
192 their blood flow distribution. An example of this phenomenon was studied by Animut and
193 Chandler (1996) in ewes describing a 25 % decrease on the mammary blood flow during
194 treadmill exercise (27). In contrast, Segers et al. (2001) developed a purely mathematical
195 model, for the estimation of stroke volume during strongly differing hemodynamic
196 conditions in sheep. At maximum O₂ consumption, 87 % of the cardiac output supplies the
197 skeletal muscles in miniature pigs (28). The measured average relative cardiac output
198 values ($2.3 \text{ dm}^3 / (\text{L} * \text{min}^{-1})$) are similar to the corresponding data of the native slow growing
199 Mangalica pig ($2.8 \text{ dm}^3 / (\text{L} * \text{min}^{-1})$ at 30 kg live weight) (14). This favorably low value
200 refers to a well-balanced cardiovascular system characteristic for this semi-intensive sheep
201 breed.

202

203 A dynamic MR imaging protocol of the sheep heart was developed in our methodological
204 experiment. The preconditioning, the specific details of ECG measurement and MR
205 imaging were elaborated. The method combined with CT imaging process of the total body
206 gives the unique opportunity to study the skeletal musculature quantitatively together with
207 the heart performance in a non-invasive manner.

208

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291 muscles of miniature swine during exercise. *J Appl Physiol* 1987; 62: 1285-1298.
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293
294

295 **Table 1 Some characteristic data concerning lamb heart performance**

296

	LVEDV	LVESV	LVSV	LVEF	LVMass	HR	CO	Septum	Anterior	Lateral	Posterior
	ml	ml	ml	%	g	b/min	L/min	mm	mm	mm	mm
Average	43	11.2	31.8	77.9	63.5	89	2.75	13.6	11.7	11.7	14.2
SD	5.6	1.8	3.8	1.8	5.6	12	0.16	0.0	0.1	0.3	0.1

297

298 Where: LVEDV = left ventricular end-diastolic volume, LVESV = left ventricular end-systolic volume,
 299 LVSV = left ventricular stroke volume, LVEF = left ventricular ejection fraction, LVMass = left ventricular
 300 mass, HR = heart rate, CO = cardiac output

301

302 **Table 2 Related cardiac output data**

303

	Muscle volume	Body surface (BS)	CO related to BS	Relative CO
	(dm³)	(dm²)	dm² / (L * min⁻¹)	dm³ / (L * min⁻¹)
Average	6.4	50.3	18.3	2.3
SD	0.79	5.5	3.1	0.26

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