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## SURFACE TREATMENT AND EXAMINATION OF GRADE 2 AND GRADE 5 TITANIUM

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15 ABSTRACT. Surface characteristics play an important role in the implant-bone integration that is 16 required for the long-term reliability of dental and orthopedic implants. In this paper, we investigate 17 the effect of acid treatment on the mass reduction and roughness of grade 2 and grade 5 Ti under 18 controlled experimental conditions. Three different etching compounds were investigated: 30% HCl, 19 85% H<sub>3</sub>PO<sub>4</sub> and the compound of 30% (COOH)<sub>2</sub>x2H<sub>2</sub>O and 30% H<sub>2</sub>O<sub>2</sub> in various treatment intervals 20 under controlled temperature. Stereo microscopy, scanning electron microscopy, roughness and weight 21 measurements were carried out on the samples. We found that neither 85% H<sub>3</sub>PO<sub>4</sub> nor the compound 22 of 30% (COOH)<sub>2</sub>x2H<sub>2</sub>O and 30% H<sub>2</sub>O<sub>2</sub> were able to remove the turning marks (furrows) from the 23 surface of Ti discs in our experimental setting. On the other hand, etching in 30% HCl yielded even 24 surfaces both on Ti grade 2 and 5 discs. We also found that etching at higher temperatures in 30%25 HCl resulted in significant mass loss. 26

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KEYWORDS: titanium, chemical etching, mass reduction, roughness.

## $_{30}^{29}$ **1.** INTRODUCTION

31 Pure titanium and titanium alloys are well-established 32 standard materials of dental and orthopedic implants 33 because of their favorable mechanical strength, chem-34 ical stability and biocompatibility [1]. Nowadays, the 35 most frequently used pure titanium is identified as 36 "commercially pure" (CP) grades 2 and 4. However, a 37 titanium-vanadium-aluminum alloy, reported as grade 38 5 or labeled as Ti6Al4V, is also commonly used. The 39 integration of titanium dental implants with the sur-40 rounding bone tissue (osseointegration) is critical to 41 ensure the long-term survival and functionality of the 42 implants [2]. The concept of osseointegration was 43 discovered by Brånemark and his co-workers. Their 44 research has had a dramatic influence on the design 45 of implants and consequently the clinical outcome of dental implant surgeries [3]. The first generation 46 47 of successfully applied titanium implants had sim-48 ple machined surfaces. Since then, implant surfaces have long been recognized to play an important role in 49 50 molecular interactions, cellular response and osseointe-51 gration. Therefore, tremendous scientific efforts have 52 been focused on the development of implants with 53 surfaces that have the capability of accelerating the 54 osseointegration and improving the long-term survival 55 of the implants. For that purpose, various methods 56 have been developed during the last 20 years, such 57 as sandblasting, acid etching, bioactive coatings, an-58 odization and, more recently, laser modification of 59 surfaces [4–6]. These implants have been extensively 60

investigated in *in vivo* experiments, including longterm clinical studies and experimental histological and biomechanical evaluation in animal models [7].

Titanium and titanium alloys are prone to develop a superficial oxide layer upon contact with oxidants [8]. The quality of the oxide layer may profoundly affect the biological behavior of titanium implants. The mechanical properties of the oxide layer, such as the thickness and roughness are known as the most important parameters that may affect the rate of osseointegration and the biomechanical properties of the devices [9]. Several types of surface treatment methods have been proposed in the scientific literature, including mechanical and chemical procedures to improve the osseointegration ability of dental implants. However, usually these publications do not disclose details about the effect of treatment parameters on the mechanical properties of titanium, but rather focus on the optimization of biological properties of the oxide layer [7–10].

## 2. Aim of the experiment

In this paper, we focus our attention on the effect of acid treatment on the mass reduction and roughness of Ti grade 2 and Ti grade 5 under controlled experimental conditions.

## **3.** The experiment

Titanium discs of 2 mm thickness and 14 mm in  $^{118}$  diameter were cut from grade 2 and grade 5 rods with  $^{119}$ 

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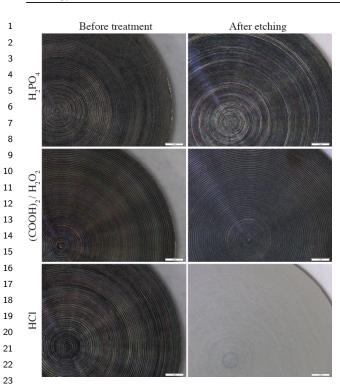


FIGURE 1. Stereo microscopic images of titanium discs before and after etching in  $H_3PO_4$ , in the compound of  $(COOH)_2 \times 2H_2O$  and  $H_2O_2$  and in 30% HCl.

geometry using a turning machine. The weight and roughness of the samples were recorded after turning.

## **3.1.** CHEMICAL ETCHING

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32 After turning, 54 pieces of Ti grade 2 and 54 pieces 33 of Ti grade 5 discs were subjected to acid etch-34 We investigated the effect of three different ing. 35 acids: 30% hydrochloric acid (HCl), 85% phospho-36 ric acid  $(H_3PO_4)$ , and the compound of 30% oxalic 37 acid ((COOH)<sub>2</sub>  $\times$  2H<sub>2</sub>O) and 30% hydrogen perox-38 ide  $(H_2O_2)$ . The etching intervals were 10, 600, 1800, 39 3600, 5400 and 7200 seconds at three temperatures: 40  $20^{\circ}$ C,  $40^{\circ}$ C and  $60^{\circ}$ C. 41

#### **3.2.** Weight measurement 43

The weight of the samples was measured (DENVER 44 Instrument APX-200, New York, United States) after 45 each etching interval. The differences in the weight of 46 the titanium discs measured before and after chemical 47 etching were calculated and plotted. 48

#### **3.3.** MICROSCOPY 50

51 Stereo microscopic (Olympus SZX16, Pennsylvania, 52 United States) images were taken of the titanium 53 discs after each etching interval in each experimental 54 group in order to record the surface pattern of the 55 samples (Figure 1). Only those samples were further 56 investigated by scanning electron microscopy (Philips 57 XL 30, Zagreb, Croatia) where the signs of turning 58 (furrows) disappeared from the surface of the discs 59 (see HCl row on Figure 1).

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### 4. Results and discussion

The stereo microscopic images showed that furrows appeared on the machined surface of titanium discs with width of 15–20 µm (Figure 1). After etching either in 85% of  $H_3PO_4$  or in the compound of 30% of  $(COOH)_2 \ge 2H_2O$  and  $30\% H_2O_2$  the surface morphology of Ti grade 2 and Ti grade 5 discs was similar to the untreated surface meaning that the turning marks (furrows) remained apparent even after the 7200 second treatment (top and middle rows of Figure 1). On the other hand, the etching in 30% HCl markedly reduced the unevenness of the surfaces both on the Ti grade 2 and the Ti grade 5 discs (bottom row on Figure 1). Thus, only HCl etched titanium discs were subjected to further investigations.

76 Concerning the treatment parameters, such as time 77 and temperature, the Ti grade 2 discs that were 78 treated in HCl at 40°C for 1800 seconds and those that were treated in HCl at  $60^{\circ}$ C for 1800 seconds 79 80 showed even surface patterns (Figure 2). However, 81 we found a considerable difference in the dissolution 82 profiles of the Ti discs treated at 40°C and 60°C. Our findings show that increasing the temperature has a 83 84 more pronounced effect on the mass reduction of Ti grade 2 than the prolonged treatment time (Figure 3). 85

86 The same treatment parameters were found to be 87 favorable to create even surfaces on Ti grade 5 discs as 88 on Ti grade 2 discs. The etching of Ti grade 5 in HCl at 40°C for 1800 seconds completely removed the furrows 89 from the surface of the discs (see Figure 2). Increasing 90 the temperature from 40°C to 60°C yielded rough 91 surfaces within the same (1800 seconds) treatment 92 period (see Figure 2). Concerning the dissolution 93 profiles of Ti grade 5, increasing the temperature of 94 the 30% HCl etchant resulted in more intense mass 95 reduction of the Ti grade 5 than Ti grade 2 discs 96 (Figure 3). 97

Interestingly, higher temperatures increased the dissolution rate of both the Ti grade 2 and Ti grade 5 samples irrespective to the composition of the etchant 100 at 60°C. Ti grade 5 showed higher dissolution rates 101 than Ti grade 2 discs and the effect of increased tem-102 perature was higher this case than on pure titanium 103 (Figure 4). 104

## **5.** CONCLUSION

107 The creation of micro-rough oxide layers on the sur-108 face of medical grade titanium in order to support 109 its osseointegration may be achieved at the cost of 110 considerable material loss depending on the chemi-111 cal composition of the titanium. Ti grade 5 shows 112 higher dissolution rates than Ti grade 2 that might 113 be attributed to the potential difference of its alloying 114 compounds creating an electrochemical cell where the etchant also acts as an electrolyte. From a practi-115 116 cal point of view, the uncontrolled etching may ad-117 versely affect the fine geometrical structures of den-118 tal implants, like the self-tapping part of the thread. Blunted threads may cause undue mechanical stress

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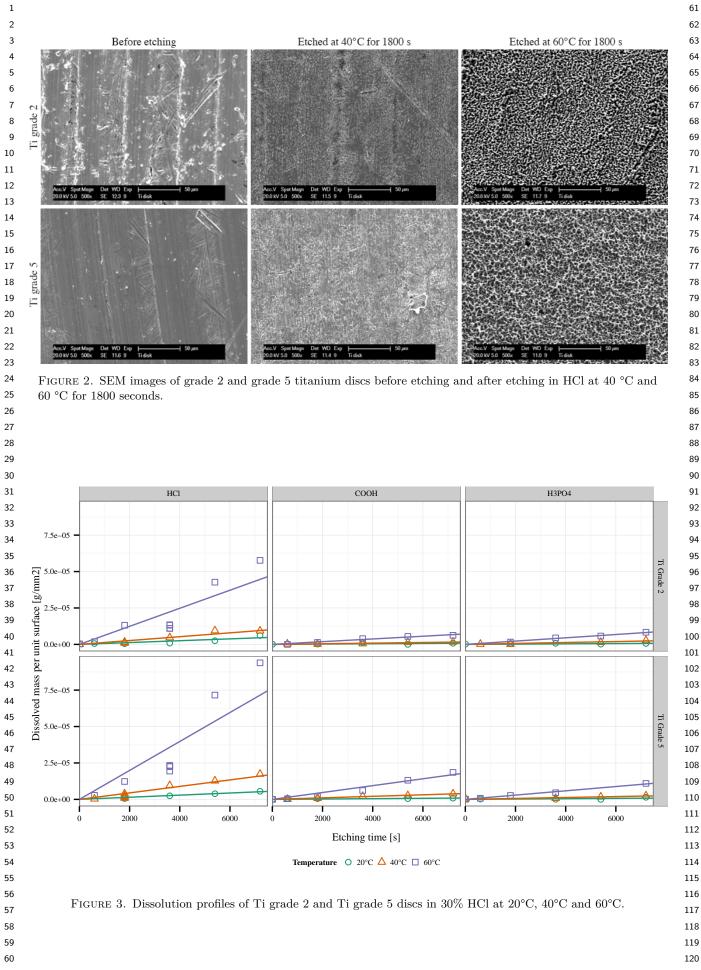
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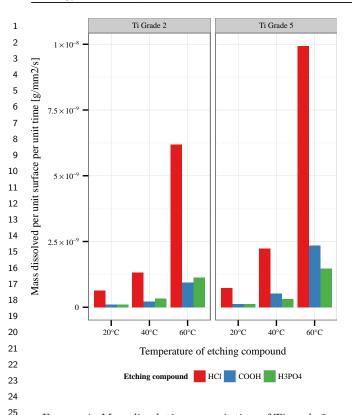


FIGURE 4. Mass dissolution per unit time of Ti grade 2 and Ti grade 5 in each etching compound.

to the bone tissue during insertion that may detri-mentally affect osseointegration. Our team plans to investigate the optimal combination of etching time and temperature in terms of material loss and surface roughness for various etchants and their effect on the fine geometry of dental implant screws. 

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